



University of
Zurich ^{UZH}

ETH

Eidgenössische Technische Hochschule Zürich
Swiss Federal Institute of Technology Zurich

KING'S
College
LONDON

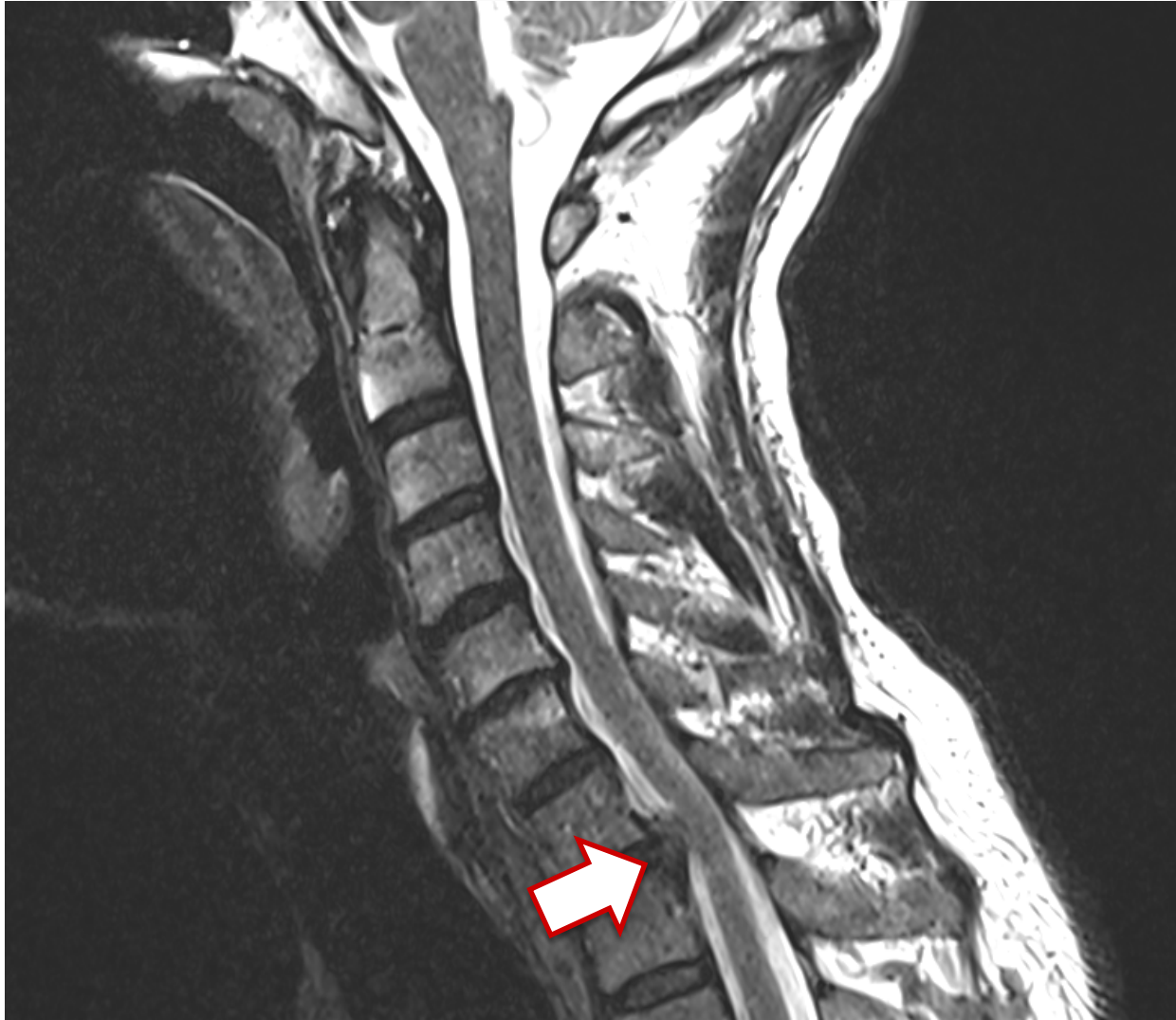
Beyond Nyquist – Accelerating Magnetic Resonance Imaging

Sebastian Kozerke

Institute for Biomedical Engineering, University and ETH Zurich, Switzerland
Imaging Sciences and Biomedical Engineering, King's College London, UK

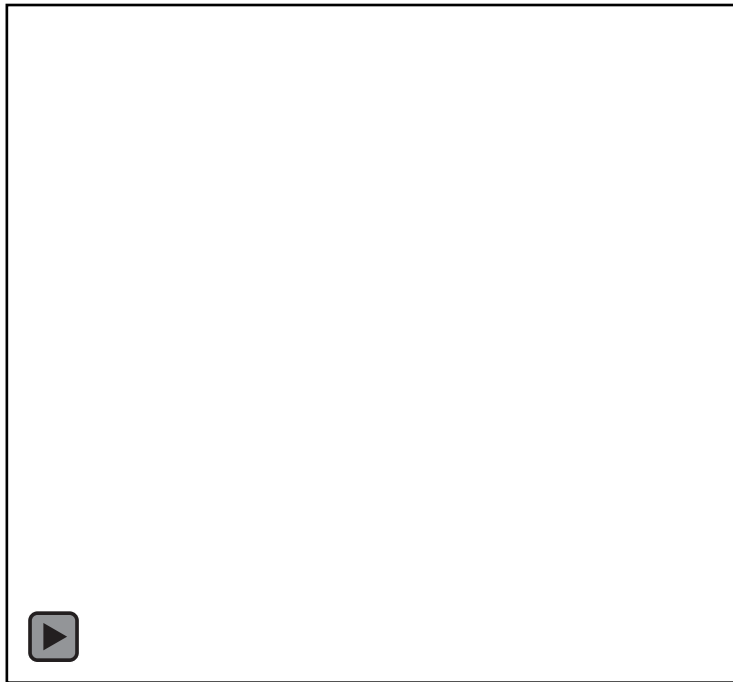


It's useful...



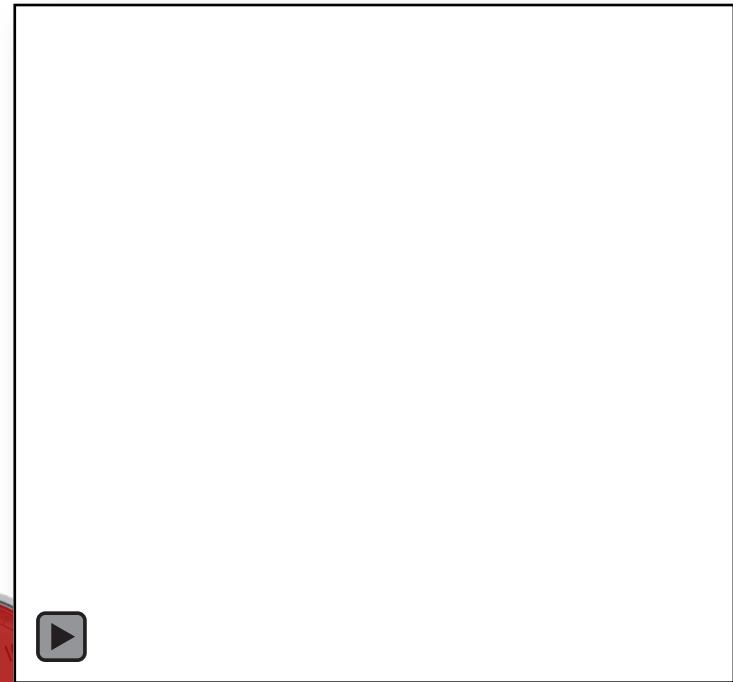
Blood flow quantification

Healthy volunteer



7D encoding (x-y-z- v_x - v_y - v_z -t)
2x2x2 mm³

Patient with dilated aorta



Magnetic Resonance Imaging

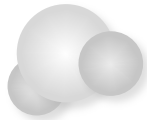
Radio transmitter



Position → Frequency



Signal source



Radio receiver



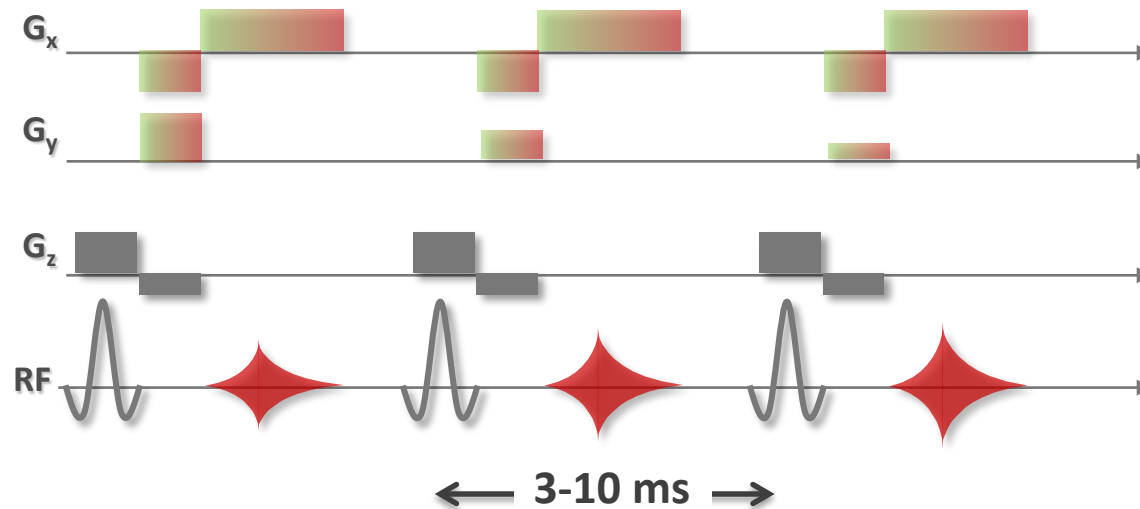
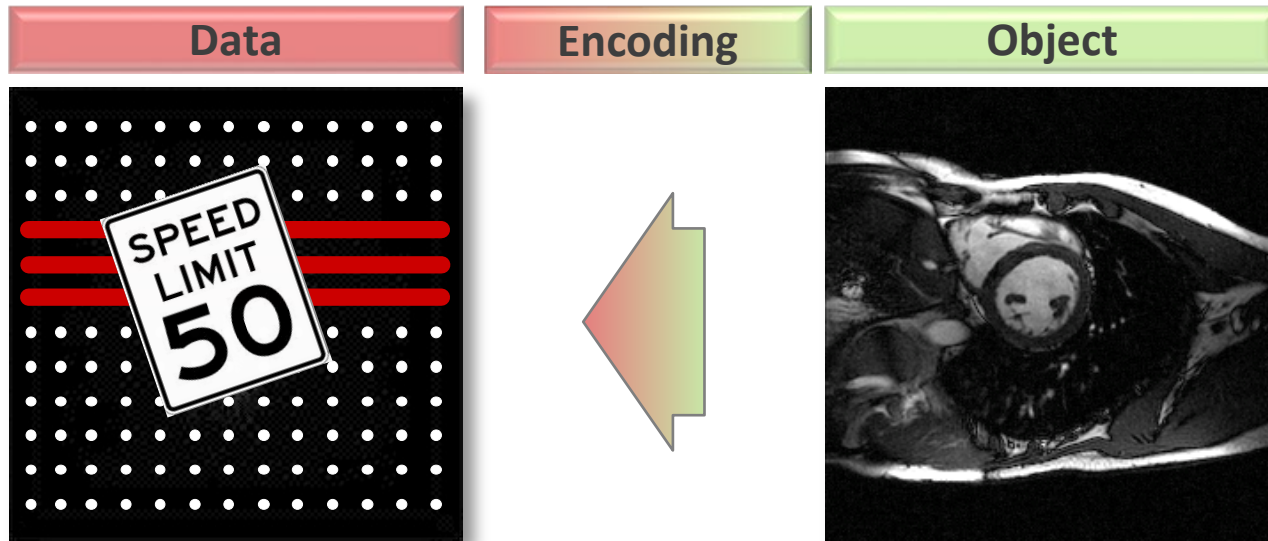
Magnetic field



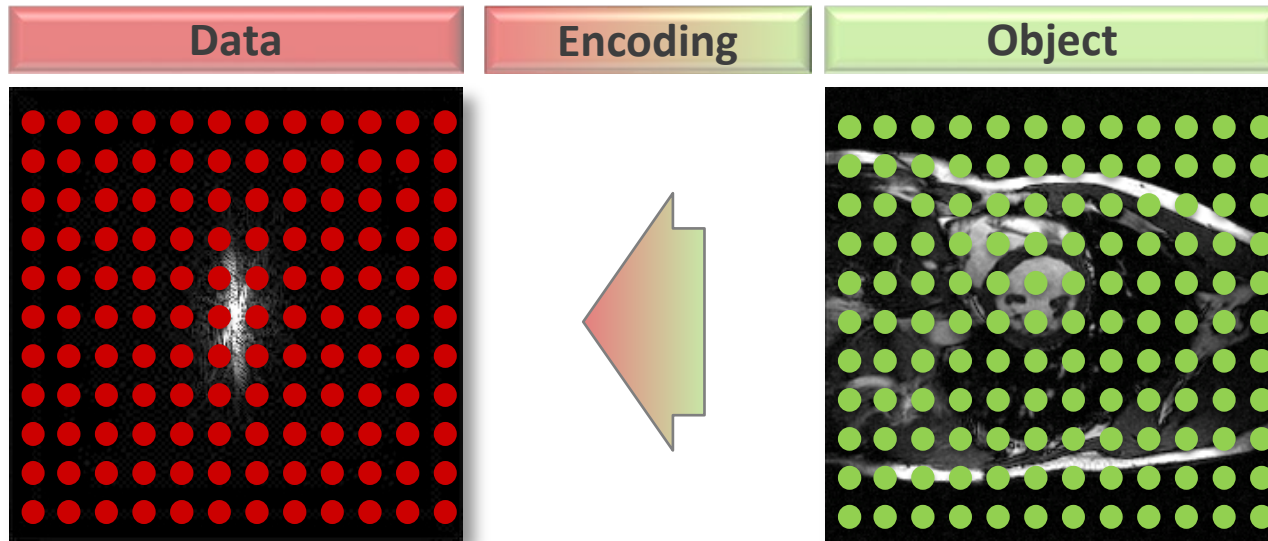
Frequency → Position



Encoding



Encoding



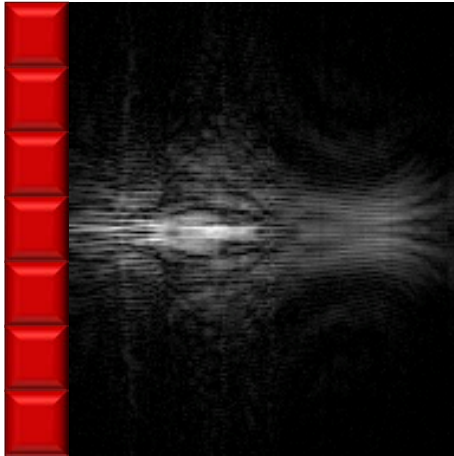
$$d_{\kappa} = \int e^{j\vec{k}_{\kappa} \cdot \vec{x}} \rho(\vec{x}) d\vec{x}$$

$$d_{\kappa} = \sum_{\xi} e^{j\vec{k}_{\kappa} \cdot \vec{x}_{\xi}} \rho(\vec{x}_{\xi})$$

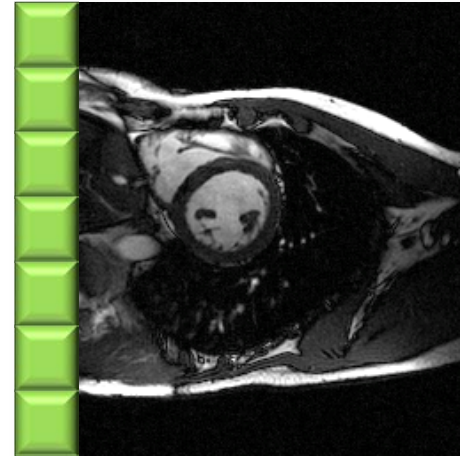
$$\vec{d} = E \vec{\rho}$$

Decoding

Data



Image



Encoding

$$\vec{d} = E \cdot \vec{\rho} + \vec{\eta}$$

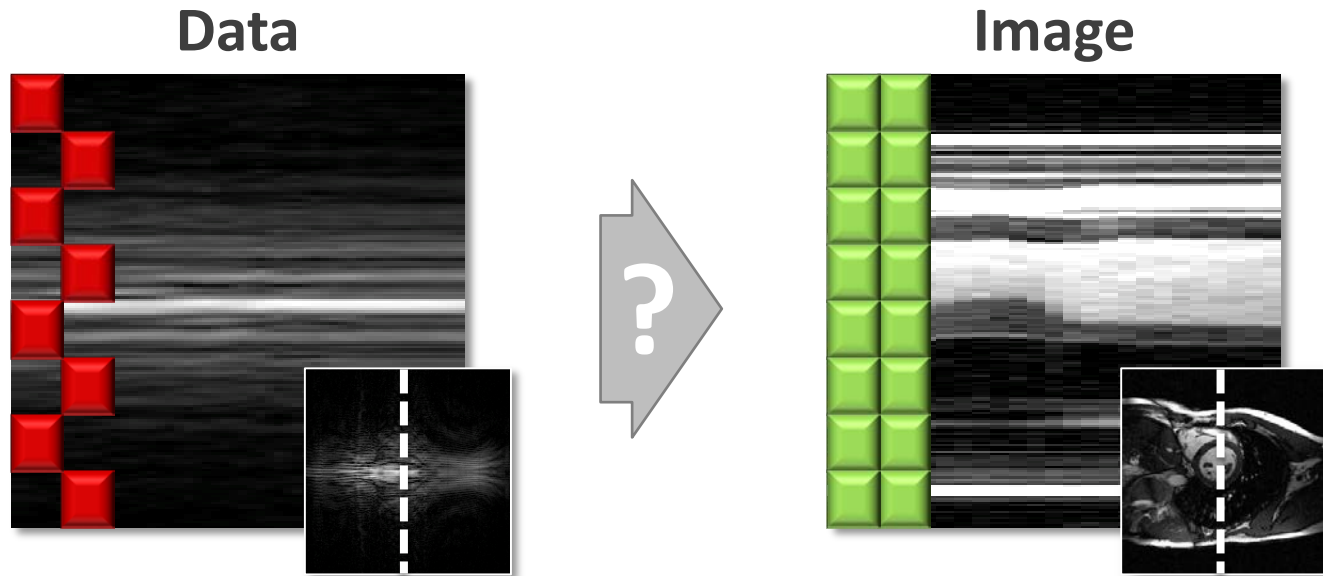


Decoding

$$\vec{i} = (E^H \Psi^{-1} E)^{-1} E^H \Psi^{-1} \cdot \vec{d}$$

$$\vec{i} \rightarrow \operatorname{argmin}_i (\vec{d} - E \cdot \vec{i})^H \Psi^{-1} (\vec{d} - E \cdot \vec{i})$$

Linear decoding



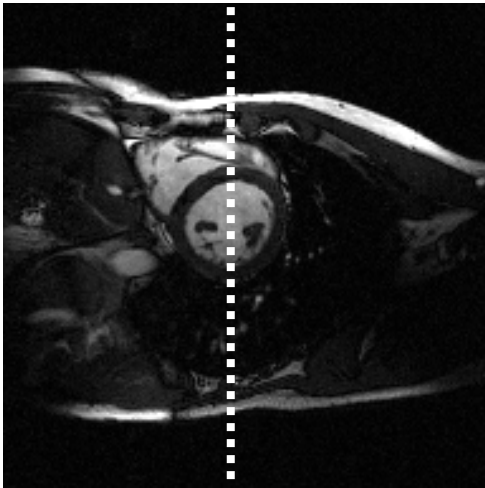
$\vec{i} \rightarrow \operatorname{argmin}_i \left\| \vec{d} - E \cdot \vec{i} \right\|_2^2$

$\vec{i} \rightarrow \operatorname{argmin}_i \left\| \vec{d} - E \cdot \vec{i} \right\|_2^2 + \lambda \left\| \Theta^{-1} \cdot \vec{i} \right\|_2^2$

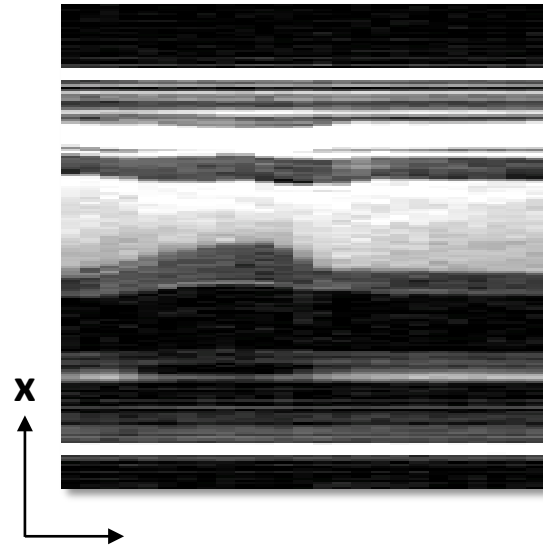
Prior info

Transform coding

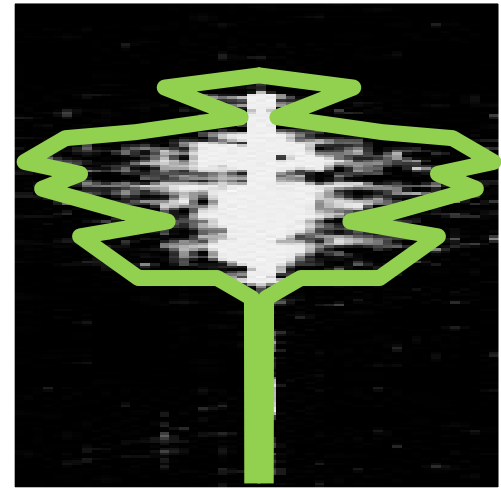
x-t space



x-t space



x-f space

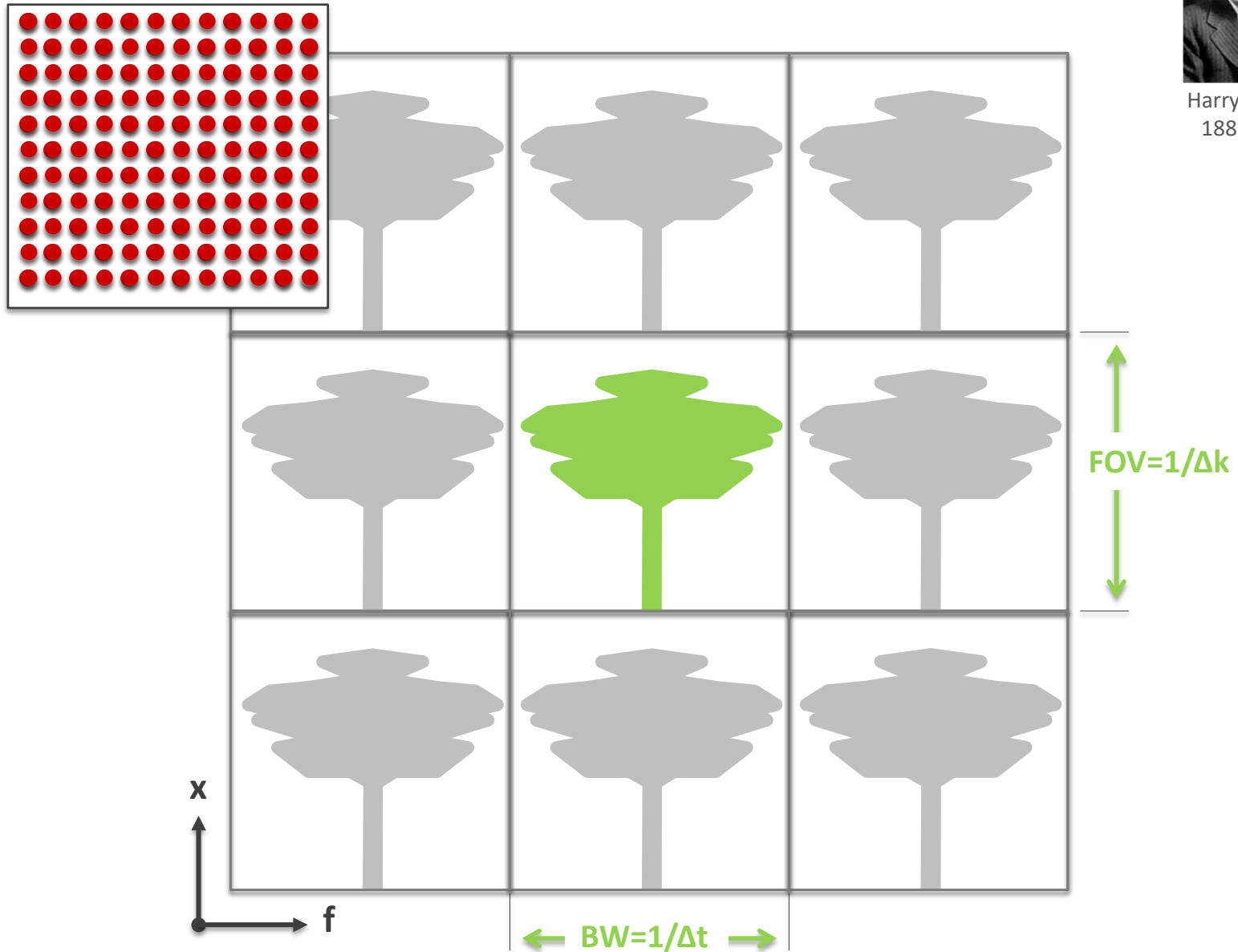


$$\tilde{\rho}(x, f_\varphi) = \sum e^{j2\pi f_\varphi t_\tau} \rho(x, t_\tau)$$

Transform coding

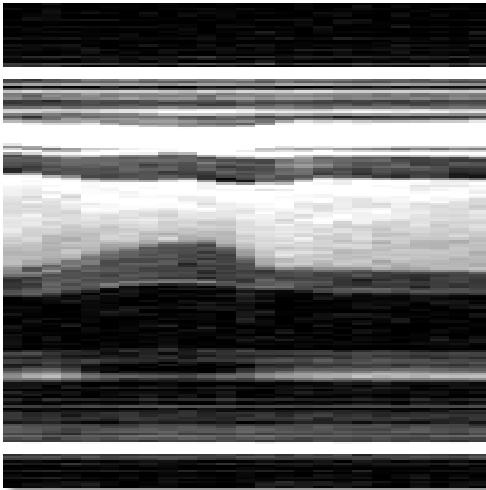


Harry Nyquist
1889-1976

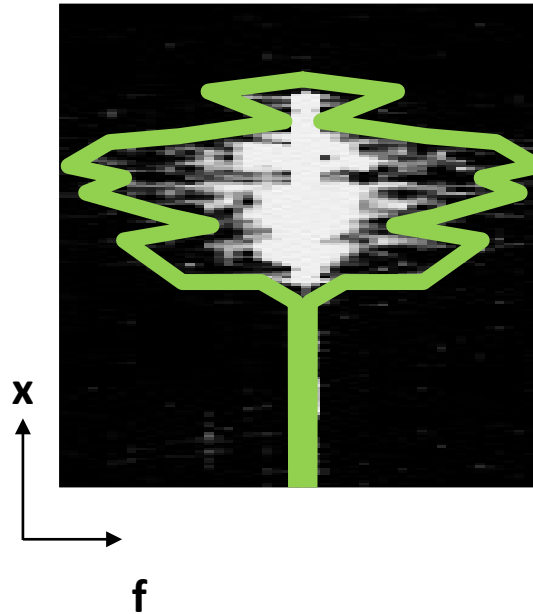


Transform coding

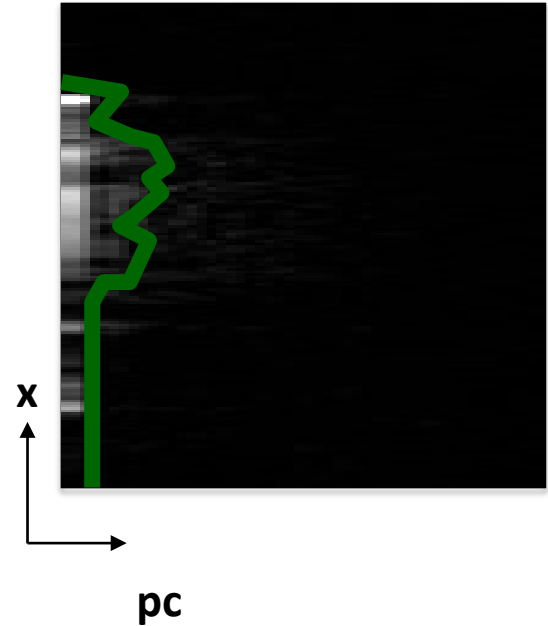
x-t space



x-f space



x-pc space



$$\tilde{\rho}(x, f) = UEV^H = \sum_{n=1}^{pc} w(x, n) b(n, f)$$

Linear decoding

Temporal regularization

$$\vec{i} \rightarrow \operatorname{argmin}_i \left\| \vec{d} - E \cdot \vec{i} \right\|_2^2 + \lambda \left\| \Phi_t \vec{i} \right\|_2^2$$

Spatiotemporal regularization

$$\vec{i} \rightarrow \operatorname{argmin}_i \left\| \vec{d} - E \cdot \vec{i} \right\|_2^2 + \lambda \left\| \Phi_{x,t} \vec{i} \right\|_2^2$$

Spatiotemporal training ($R < N_c$)

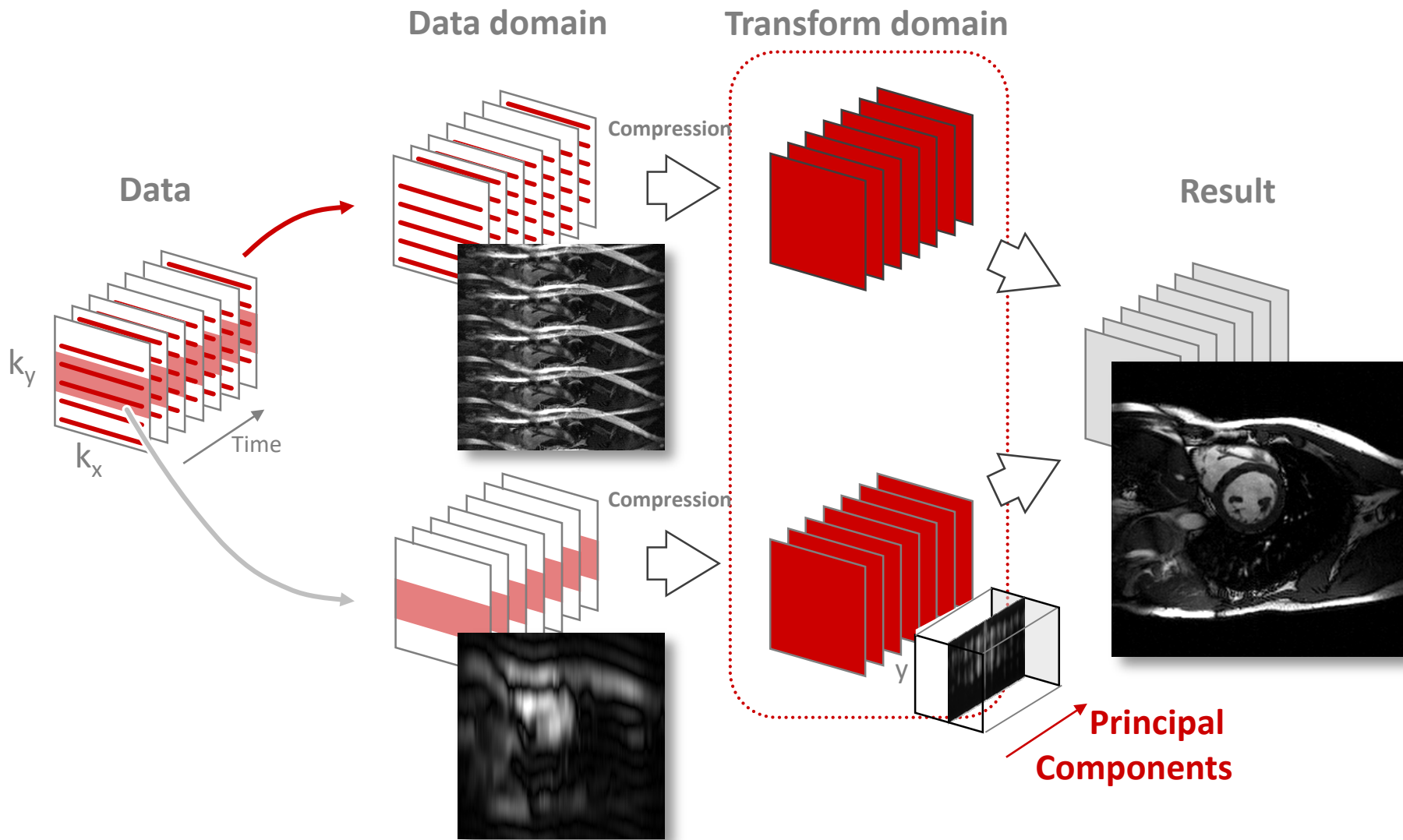
$$\vec{w} = \left(\tilde{E}^H \tilde{\Psi}^{-1} \tilde{E} + \lambda \tilde{\Theta}^{-1} \right)^{-1} \tilde{E}^H \tilde{\Psi}^{-1} \vec{d}$$

Spatiotemporal training ($R > N_c$)

$$\vec{w} = \tilde{\Theta} \tilde{E}^H \left(\tilde{E} \tilde{\Theta} \tilde{E}^H + \lambda \tilde{\Psi} \right)^{-1} \vec{d}$$

k-t PCA

k-t PCA



Nonlinear decoding

Temporal regularization

$$\vec{i} \rightarrow \operatorname{argmin}_i \left\| \vec{d} - E \cdot \vec{i} \right\|_2^2 + \lambda \left\| \Phi_t \vec{i} \right\|_2^2$$

Spatiotemporal regularization

$$\vec{i} \rightarrow \operatorname{argmin}_i \left\| \vec{d} - E \cdot \vec{i} \right\|_2^2 + \lambda \left\| \Phi_{x,t} \vec{i} \right\|_2^2$$

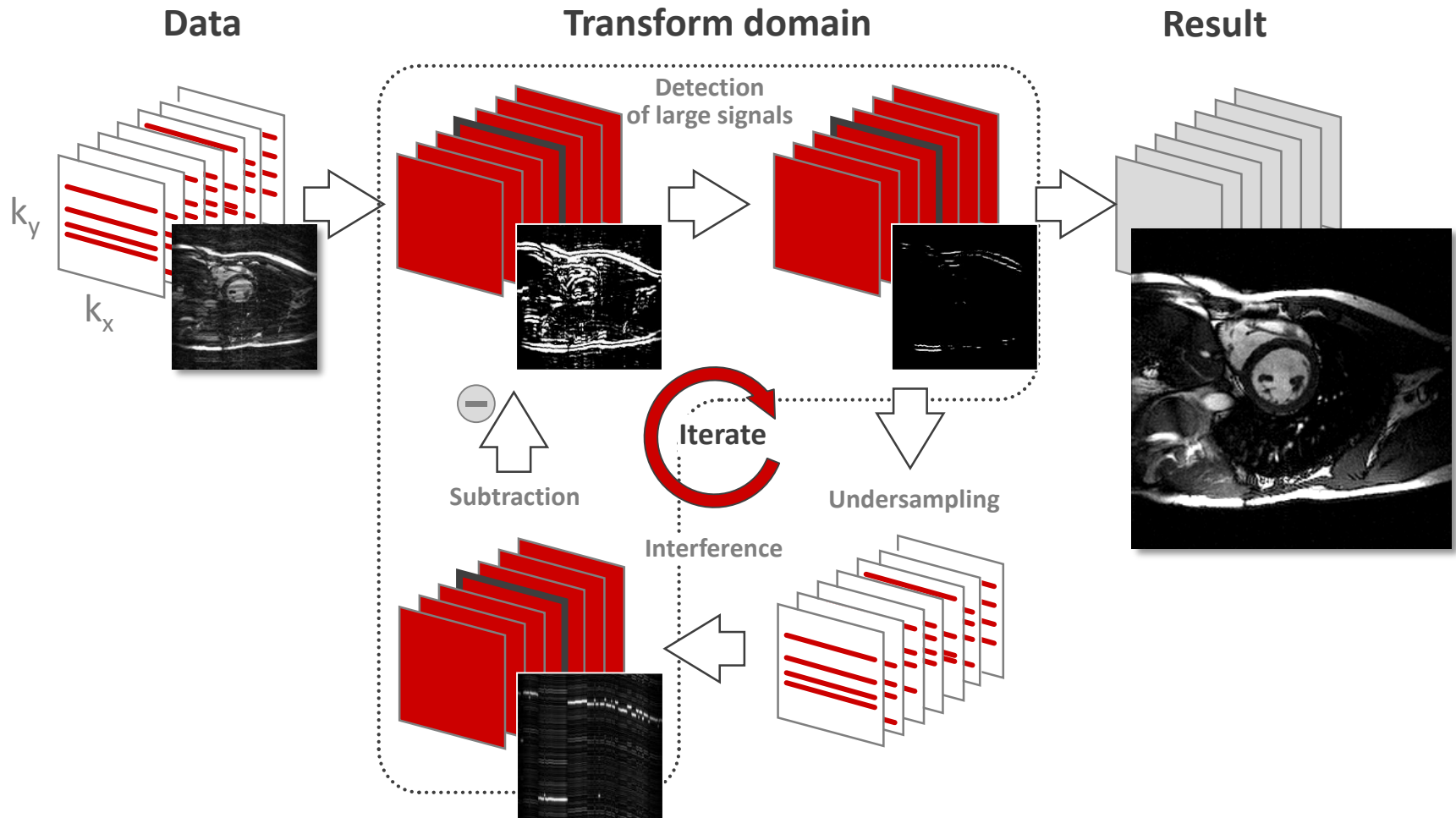
Compressed Sensing

$$\vec{i} \rightarrow \operatorname{argmin}_i \left\| \vec{d} - E \cdot \vec{i} \right\|_2^2 + \lambda \left\| \Phi_{x,f} \vec{i} \right\|_1$$

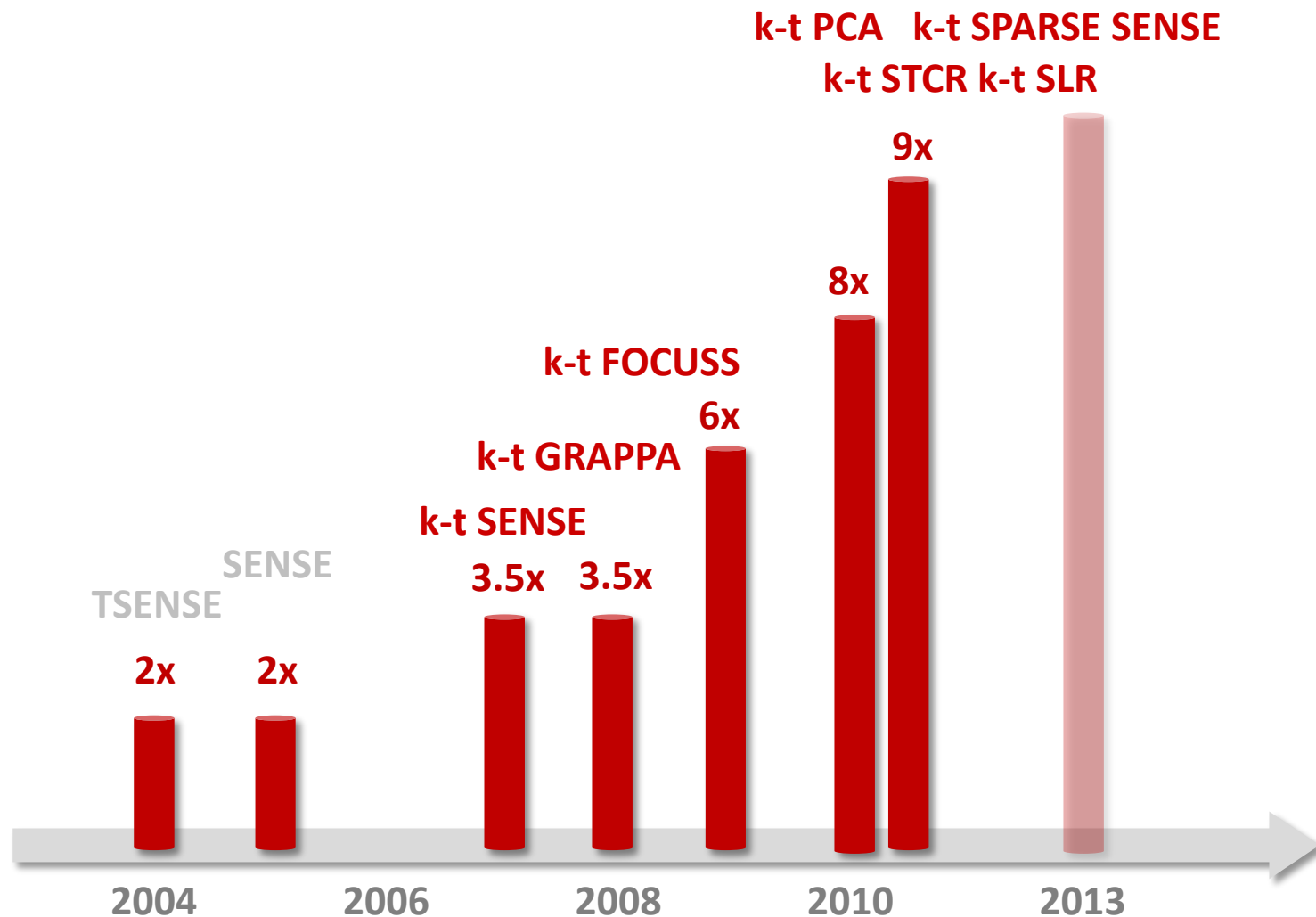
Low-rank sparse decomposition

$$\vec{i} \rightarrow \operatorname{argmin}_i \left\| \vec{d} - E \cdot (L + S) \right\|_2^2 + \lambda_L \left\| L \right\|_* + \lambda \left\| S \right\|_1$$

Compressed Sensing



Undersampling progress – Cardiac



Kellman P et al. MRM 2004
Plein S et al. Radiology 2005

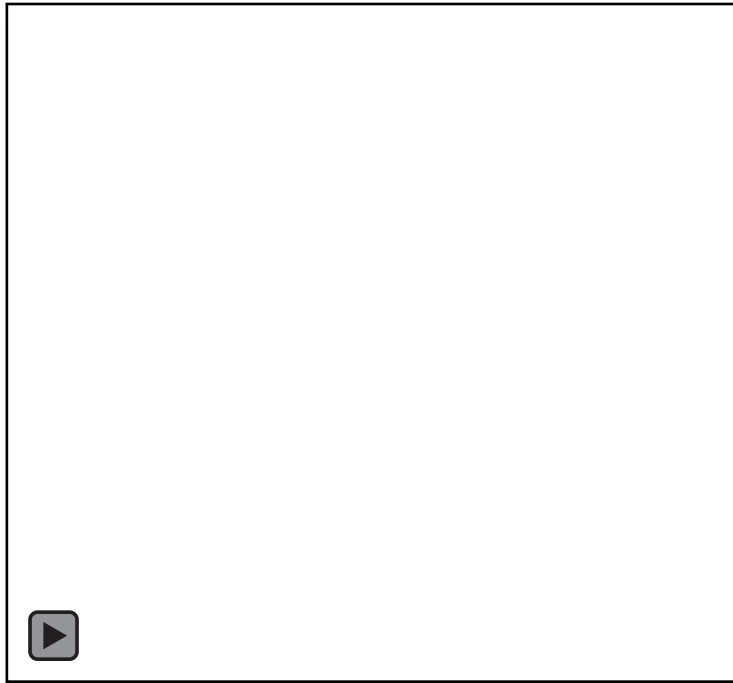
Plein S et al. MRM 2007
Jung B et al. JMRI 2008

Nayak KS et al. JCMR 2008
Vitanis V et al. MRM 2010

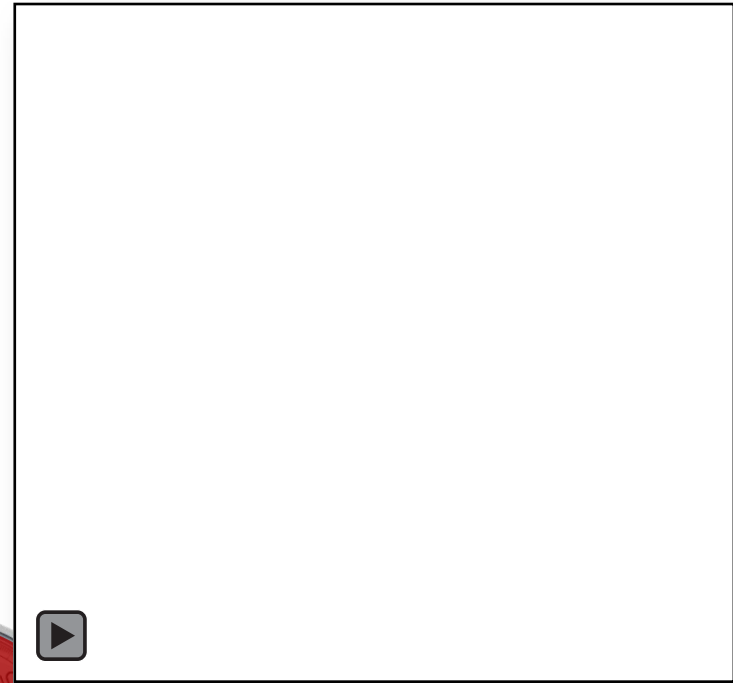
Otazo R et al. MRM 2010
Lingala SG et al. IEEE 2011

Blood flow quantification

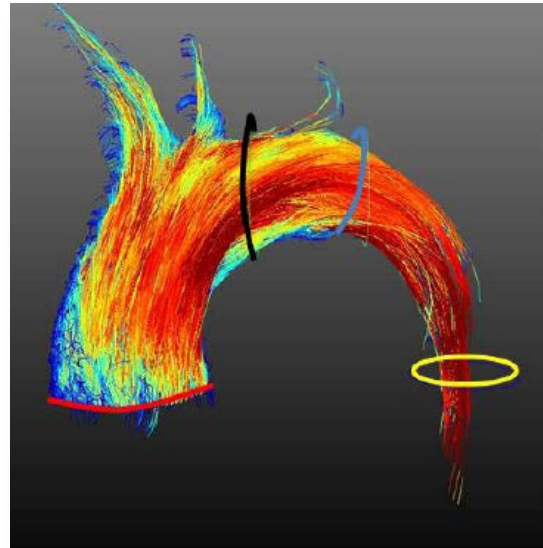
Healthy volunteer



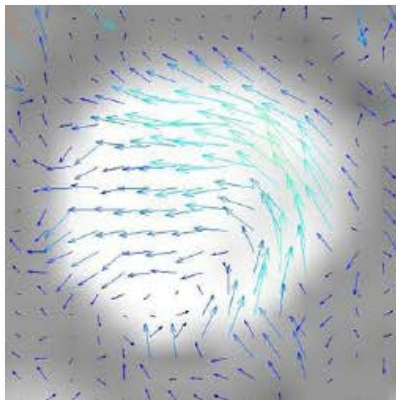
Patient with dilated aorta



Reconstruction accuracy



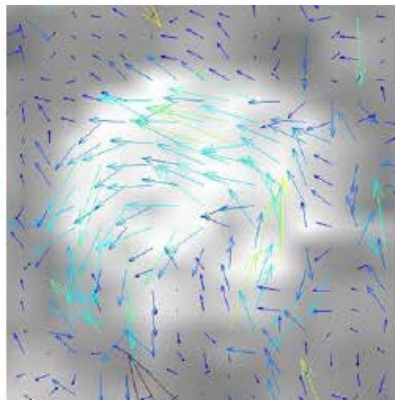
R=1



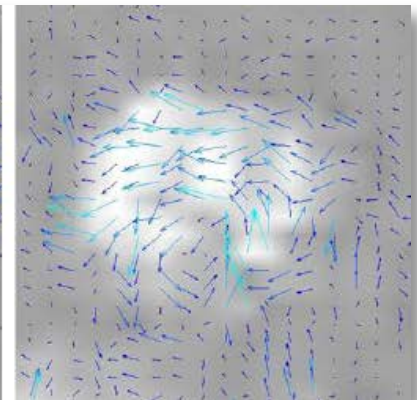
R=4



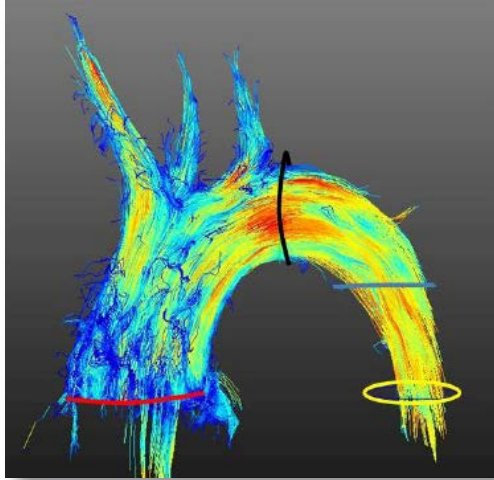
R=8



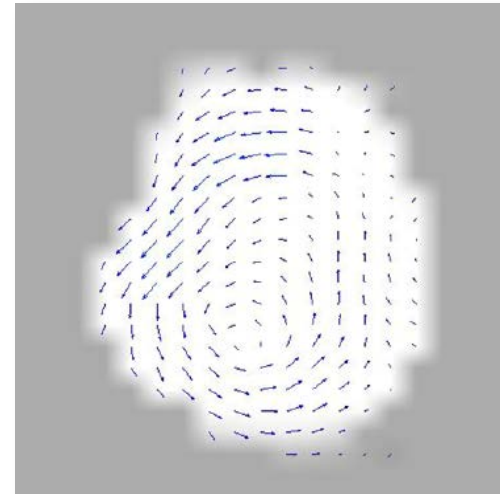
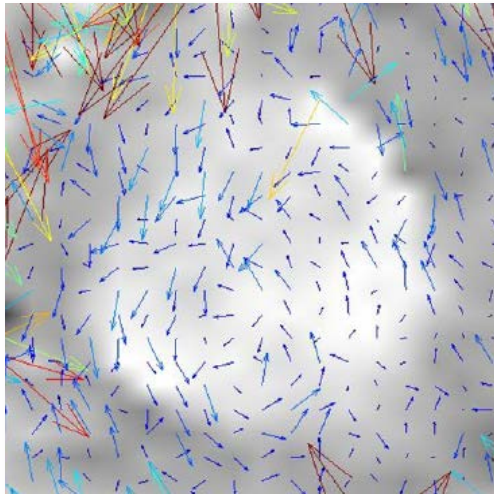
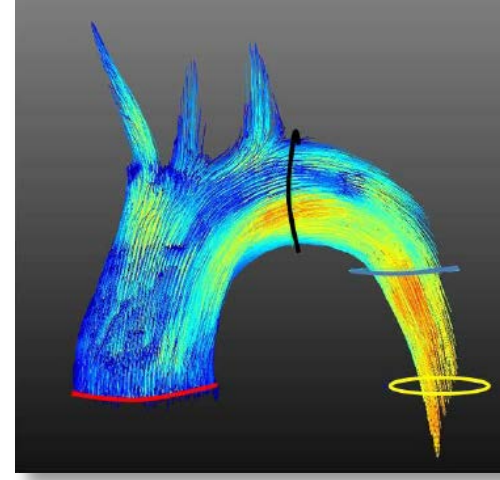
R=16



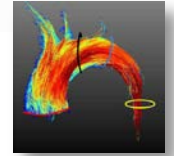
Divergence-free image reconstruction



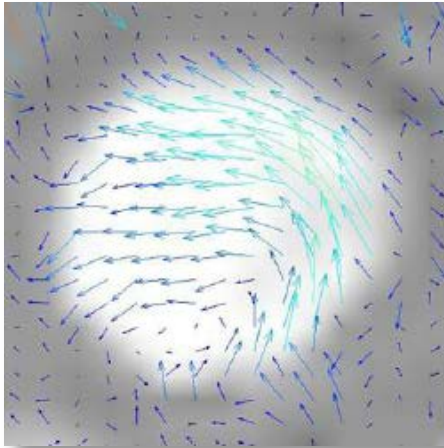
$$\text{div}(\mathbf{v})=0$$



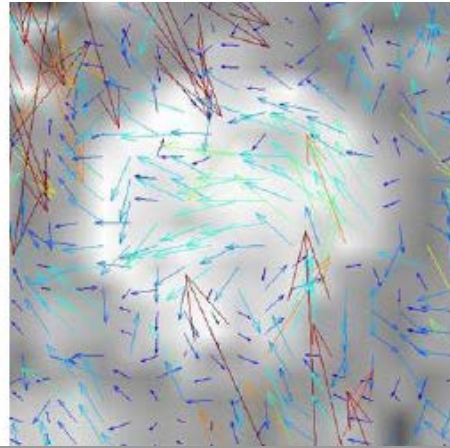
Divergence-free image reconstruction



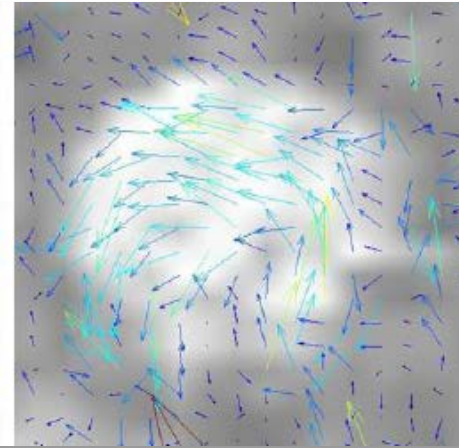
R=1



R=4



R=8



$\text{div}(\mathbf{v})=0$

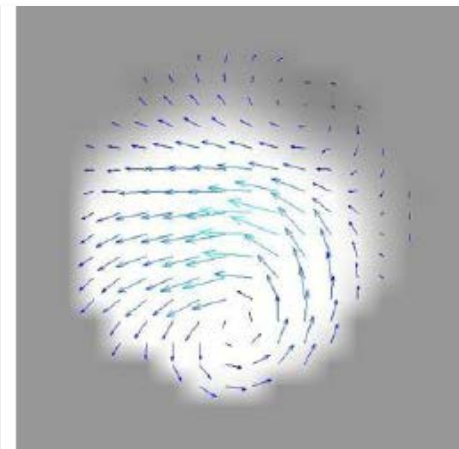
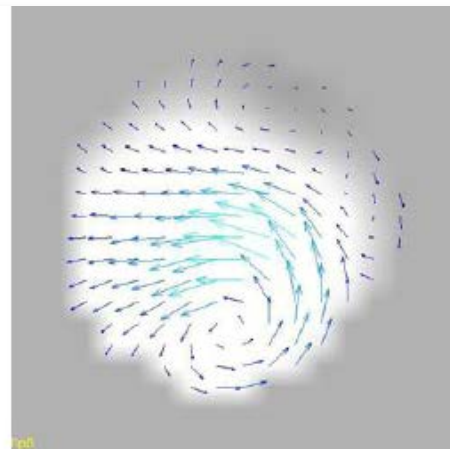
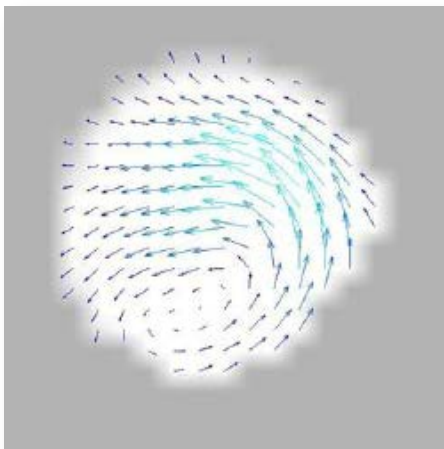
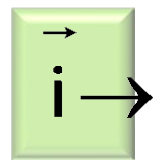
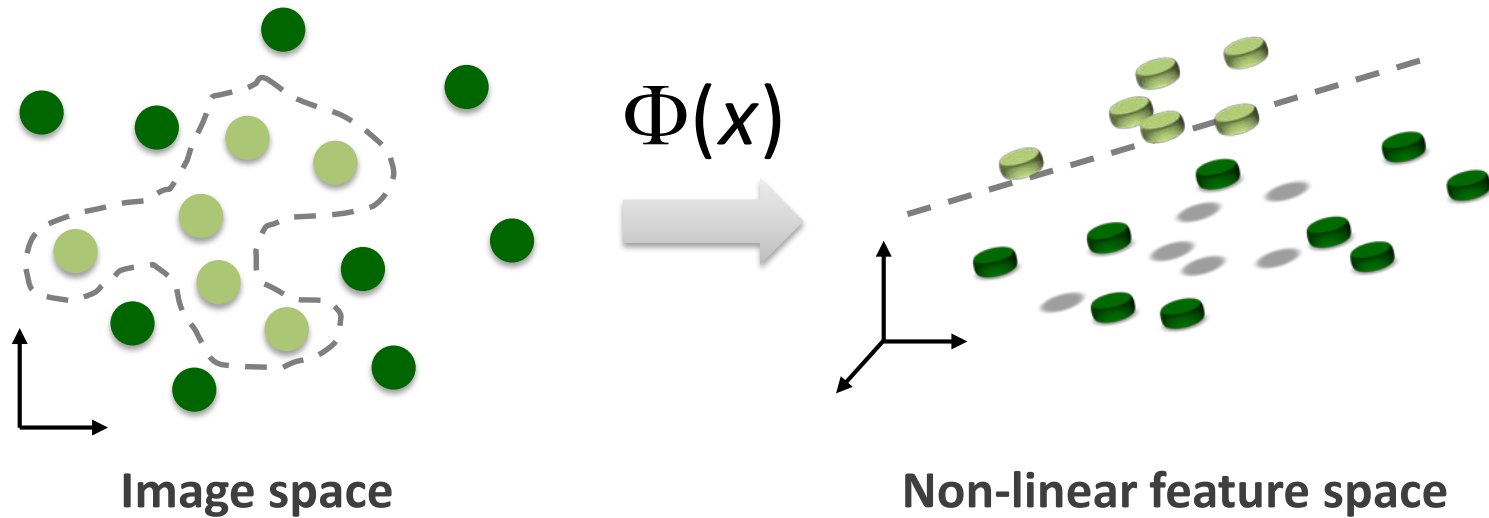
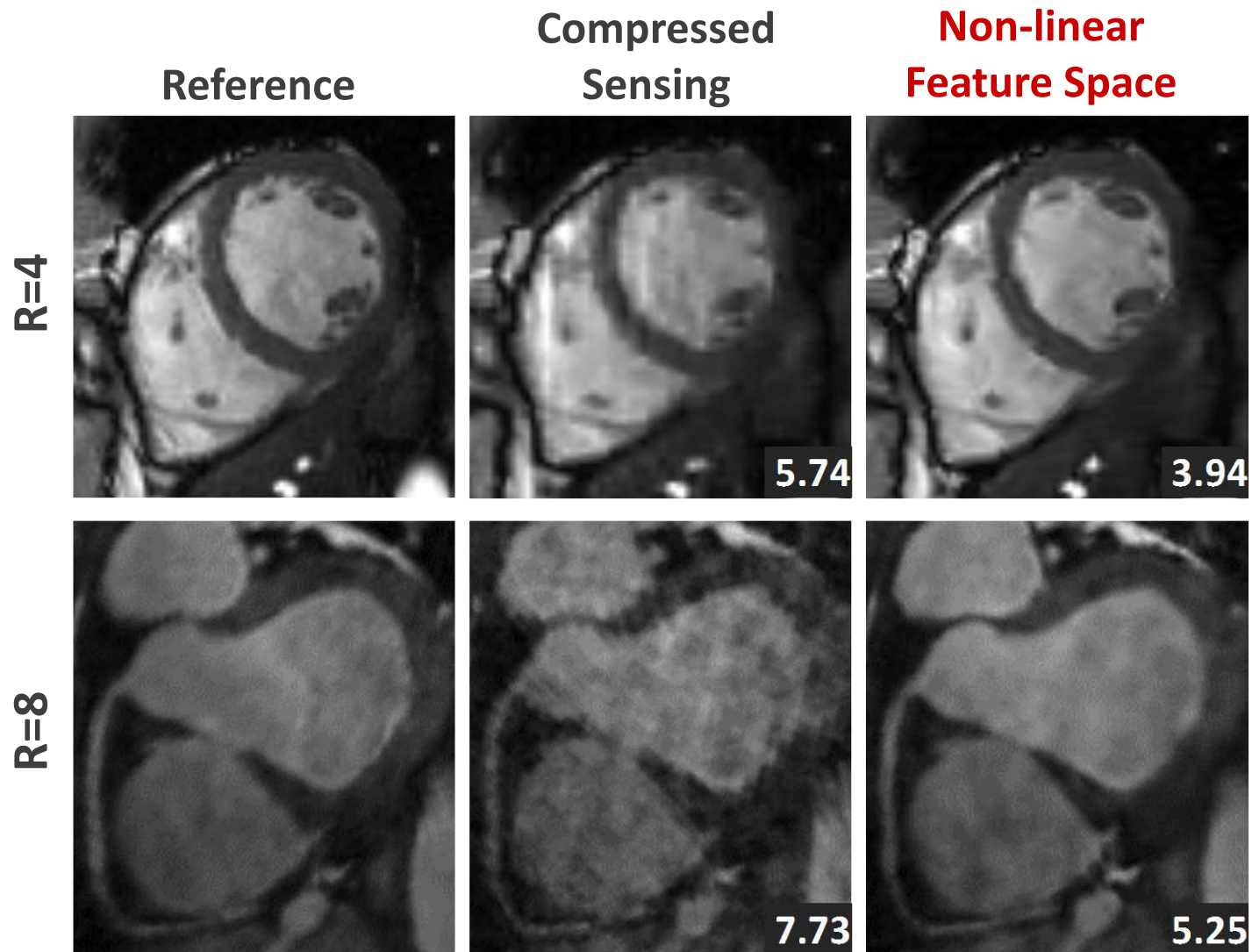


Image reconstruction in non-linear feature spaces

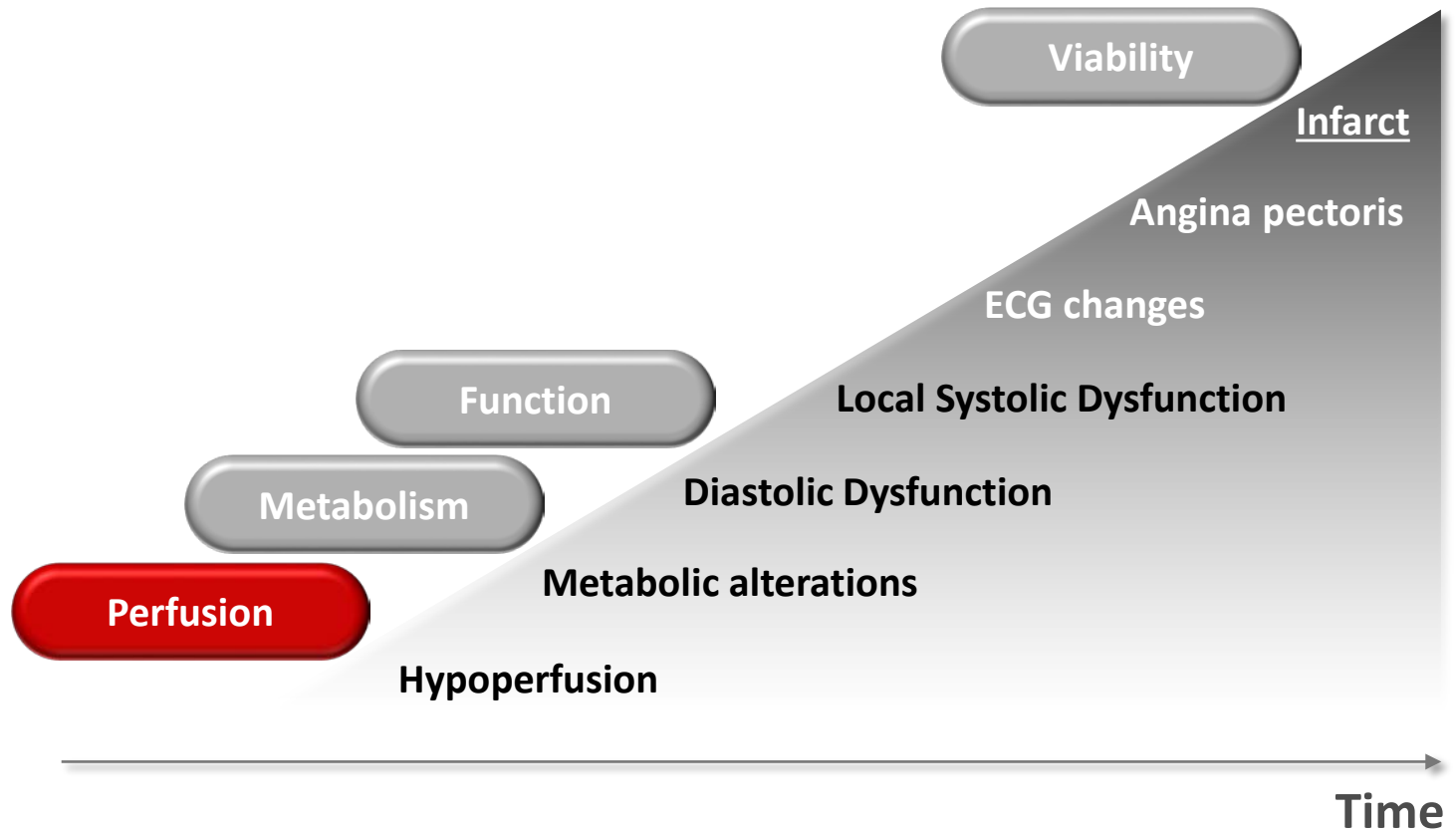


$$\vec{i}_{n+1} = \mathcal{P}_{\text{kPCA}}(\vec{i}_n - E^H(E\vec{i}_n - \vec{d}))$$

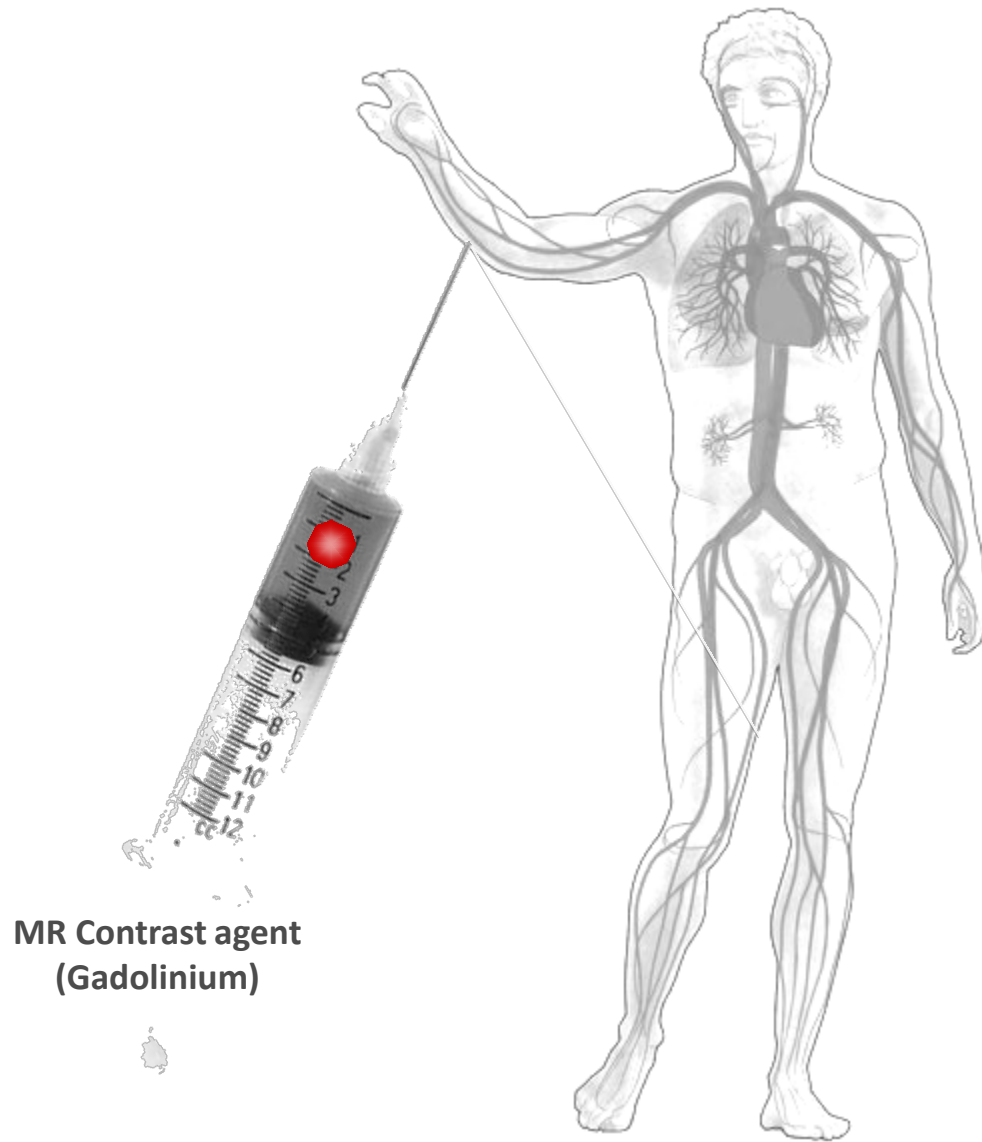
Image reconstruction in non-linear feature spaces



Ischemic cascade



3D dynamic perfusion imaging



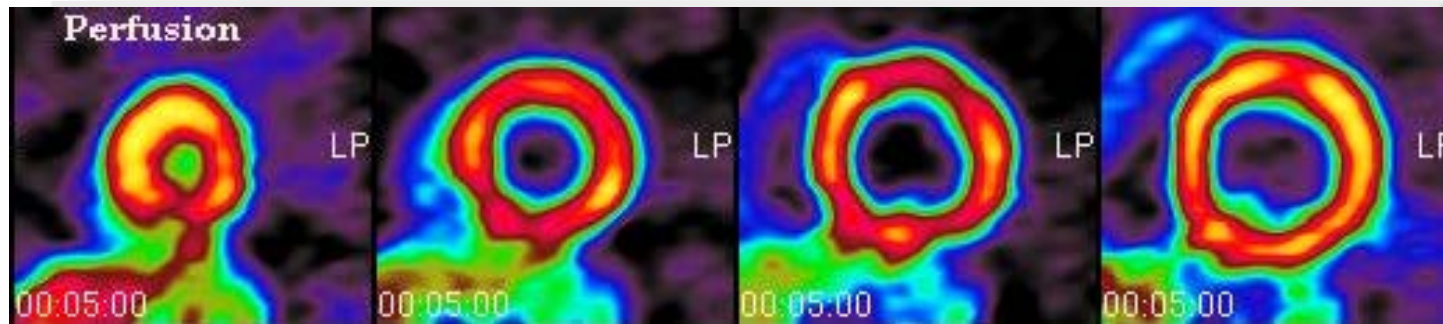
2D Perfusion imaging

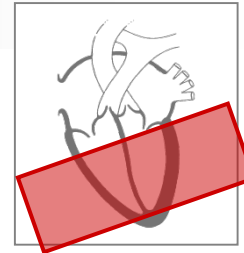


5x 2D k-t SENSE (1.1 x 1.1 mm²)



Stress PET





10x k-t PCA (2.2x2.2x10 mm³)



3D Perfusion Multi-centre study

Multicenter Evaluation of Dynamic Three-dimensional Whole-heart Myocardial Perfusion Imaging at 3.0 Tesla for the Detection of Coronary Artery Disease

Robert Manka^{1,2}, Rolf Gebker³, Lukas W.

¹University and
²Germany, ⁴Kin

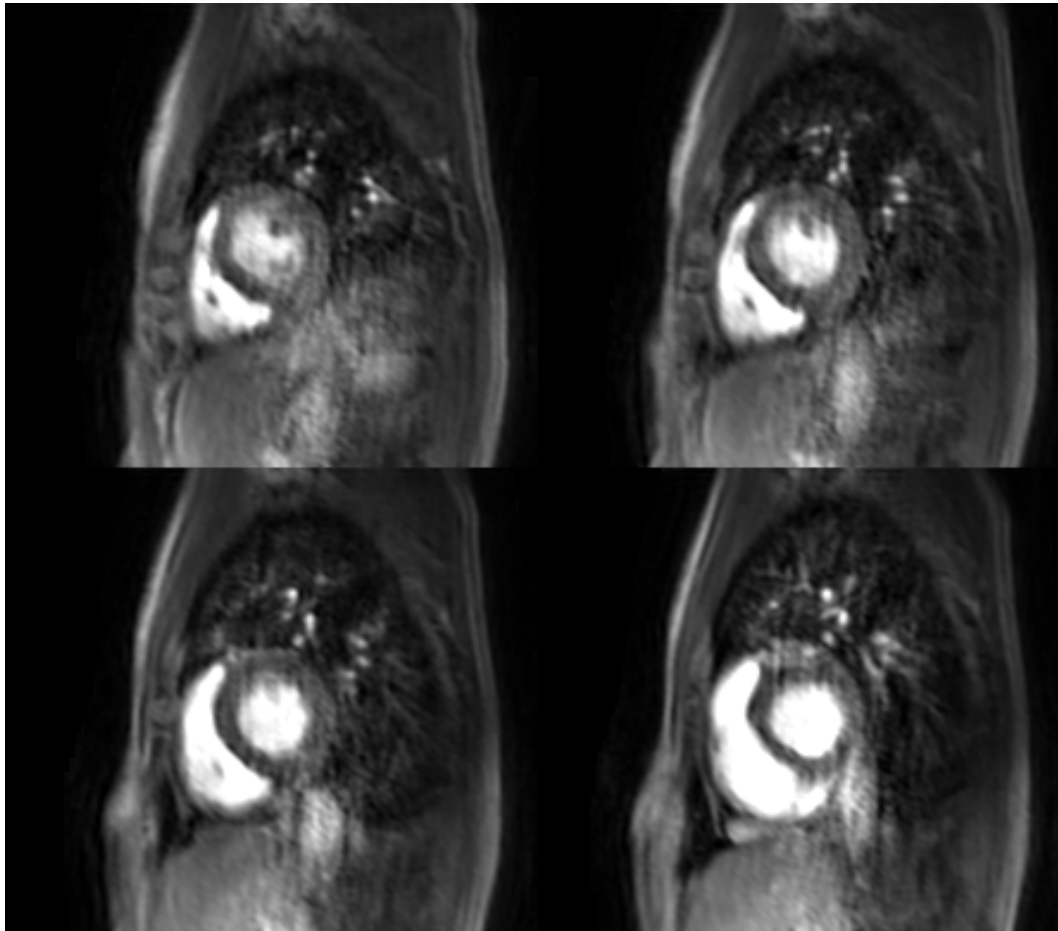
N=150	CMR vs. FFR	CMR vs. QCA
Sensitivity (%)	90	77
Specificity (%)	89	94
NPV (%)	88	68
PPV (%)	89	96

Imaging at 3.0
serve
tz⁶, Bernhard
te Berlin, Berlin,
Hospital RWTH

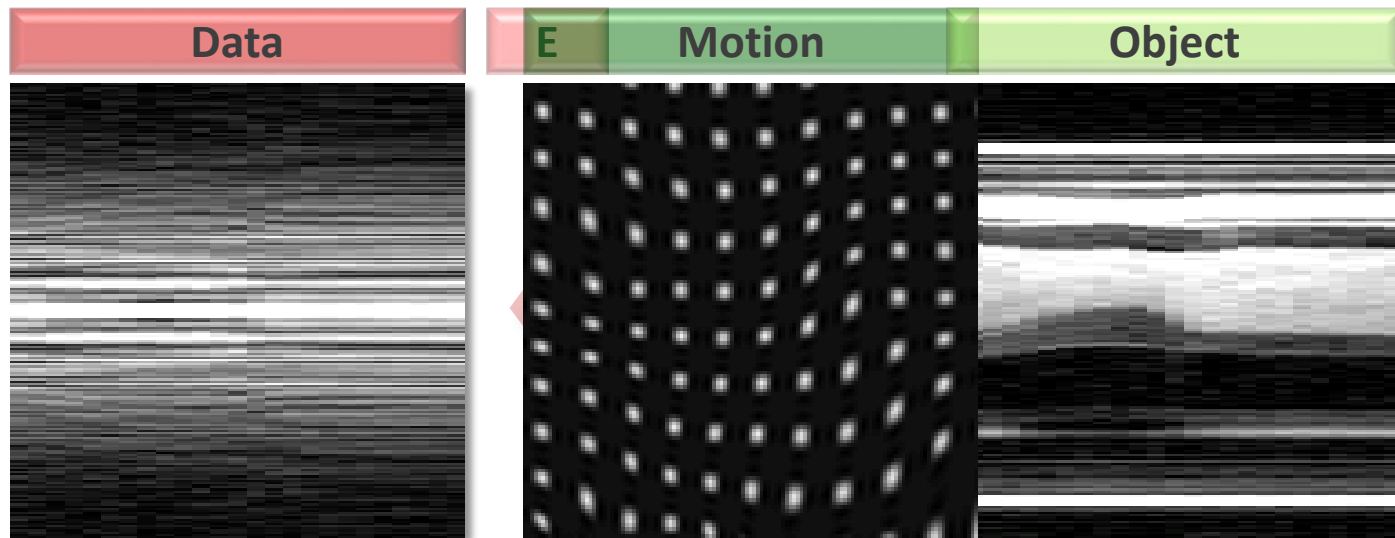


Motion artifacts

10x 3D k-t PCA (2.2 x 2.2 mm²)



Generic matrix description of motion

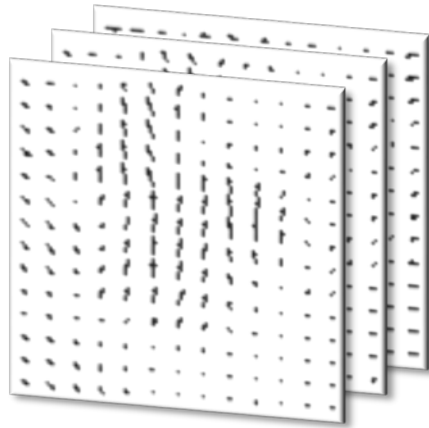


$$\vec{d} = \sum_i \underbrace{E_i T_i}_{\hat{E}} \vec{p}$$

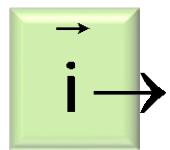
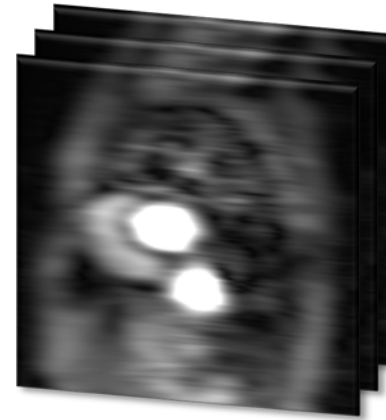
$$\vec{i} = \left(\hat{E}^H \Psi^{-1} \hat{E} + \lambda \Theta^{-1} \right)^{-1} \hat{E}^H \Psi^{-1} \vec{d}$$

Data-driven motion correction

Motion



Estimate (x-t)

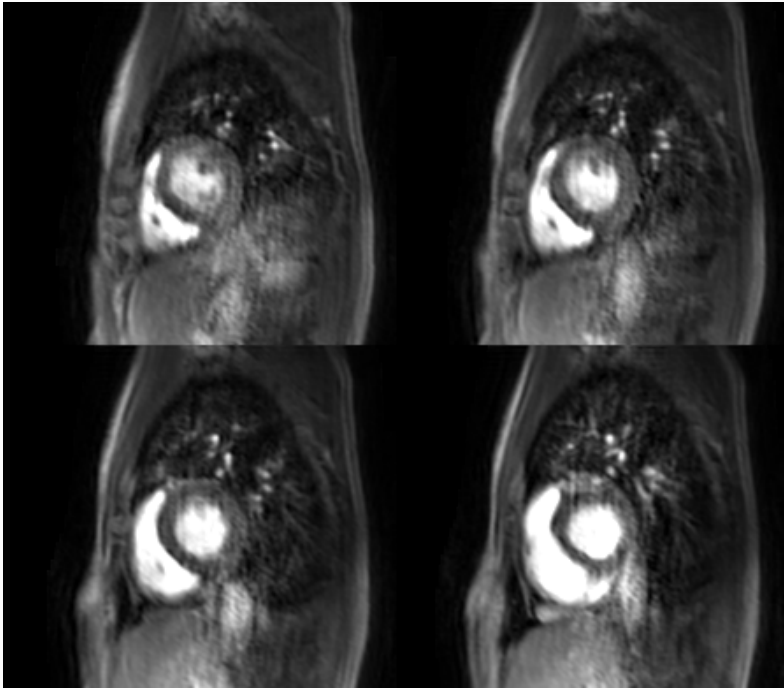


$$\operatorname{argmin}_i \left\| \vec{d} - E \cdot \vec{i} \right\|_2^2 + \lambda \left\| \left(\mathbf{T}_{x-pc} \Theta \right)^{-1} \mathbf{B}_{f \rightarrow pc} E_{t \rightarrow f} \vec{T} \vec{i} \right\|_2^2$$

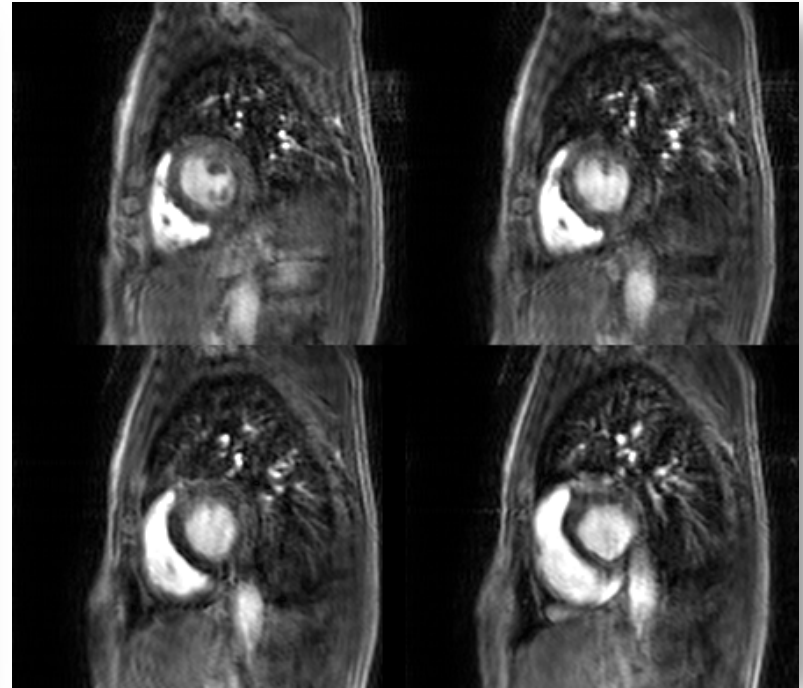
k-t PCA^{mc}

Data-driven motion correction

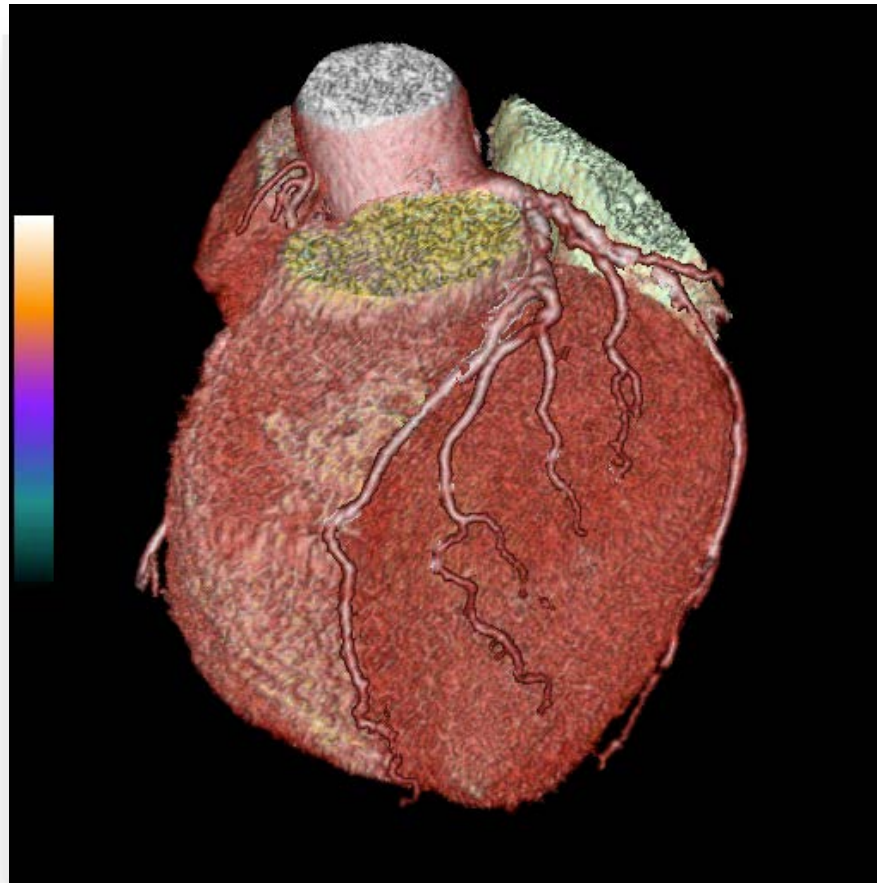
10x 3D k-t PCA



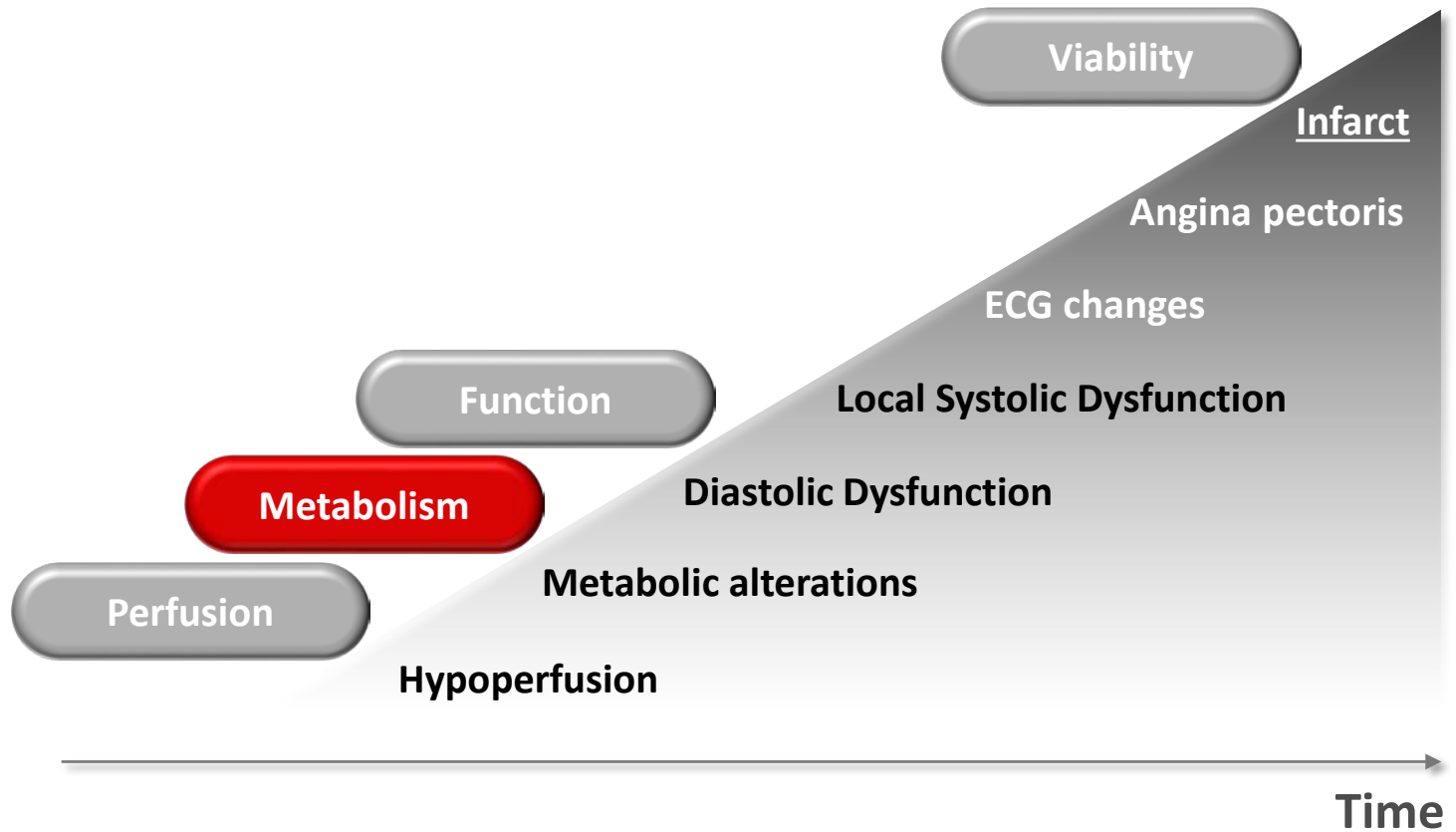
10x **3D k-t PCA^{mc}**



3D MR Perfusion + CT Angiography



Ischemic cascade



Chemical shift

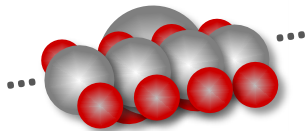
Radio transmitter



Chemical Shift → Frequency



Signal source



Radio receiver



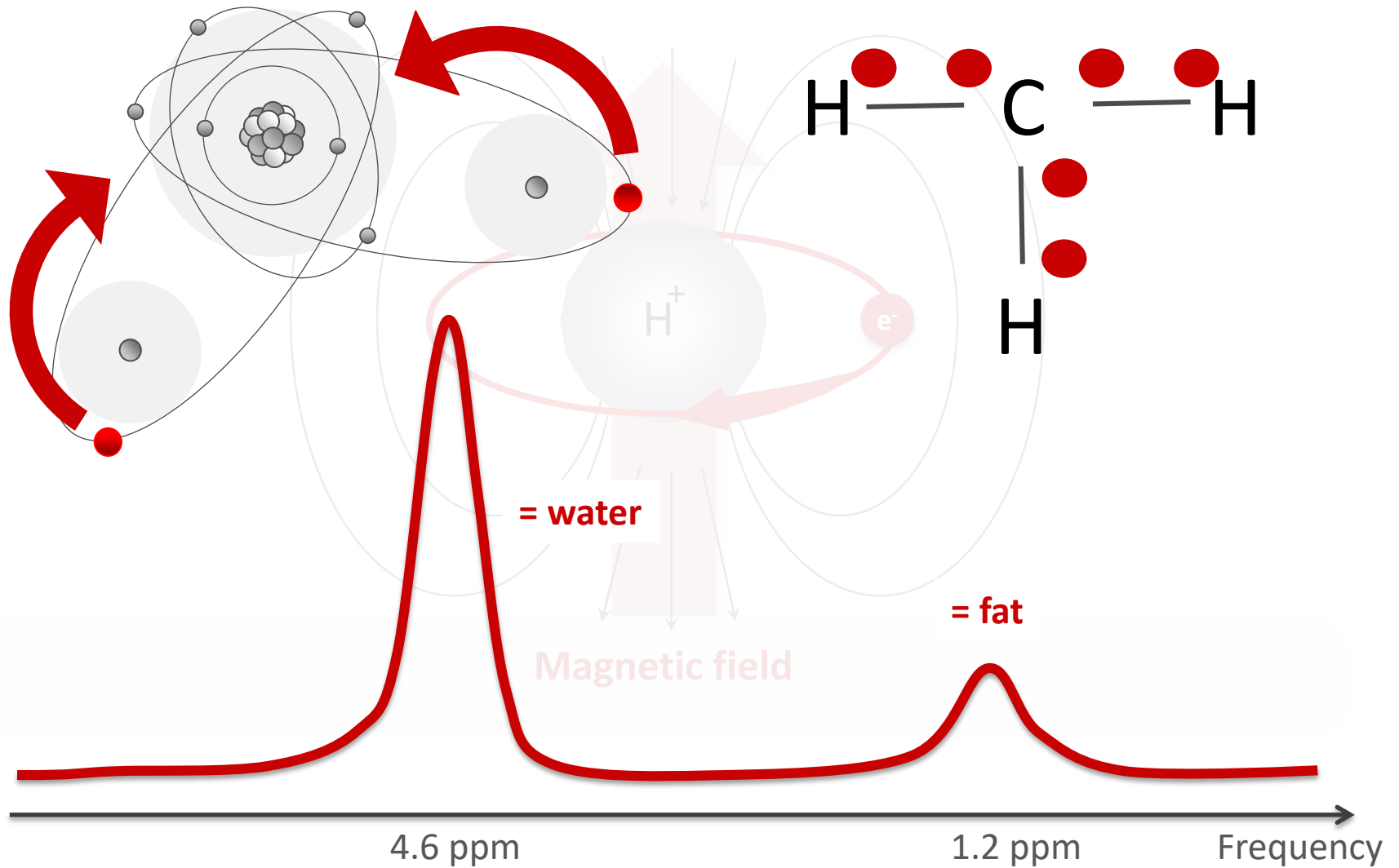
Magnetic field



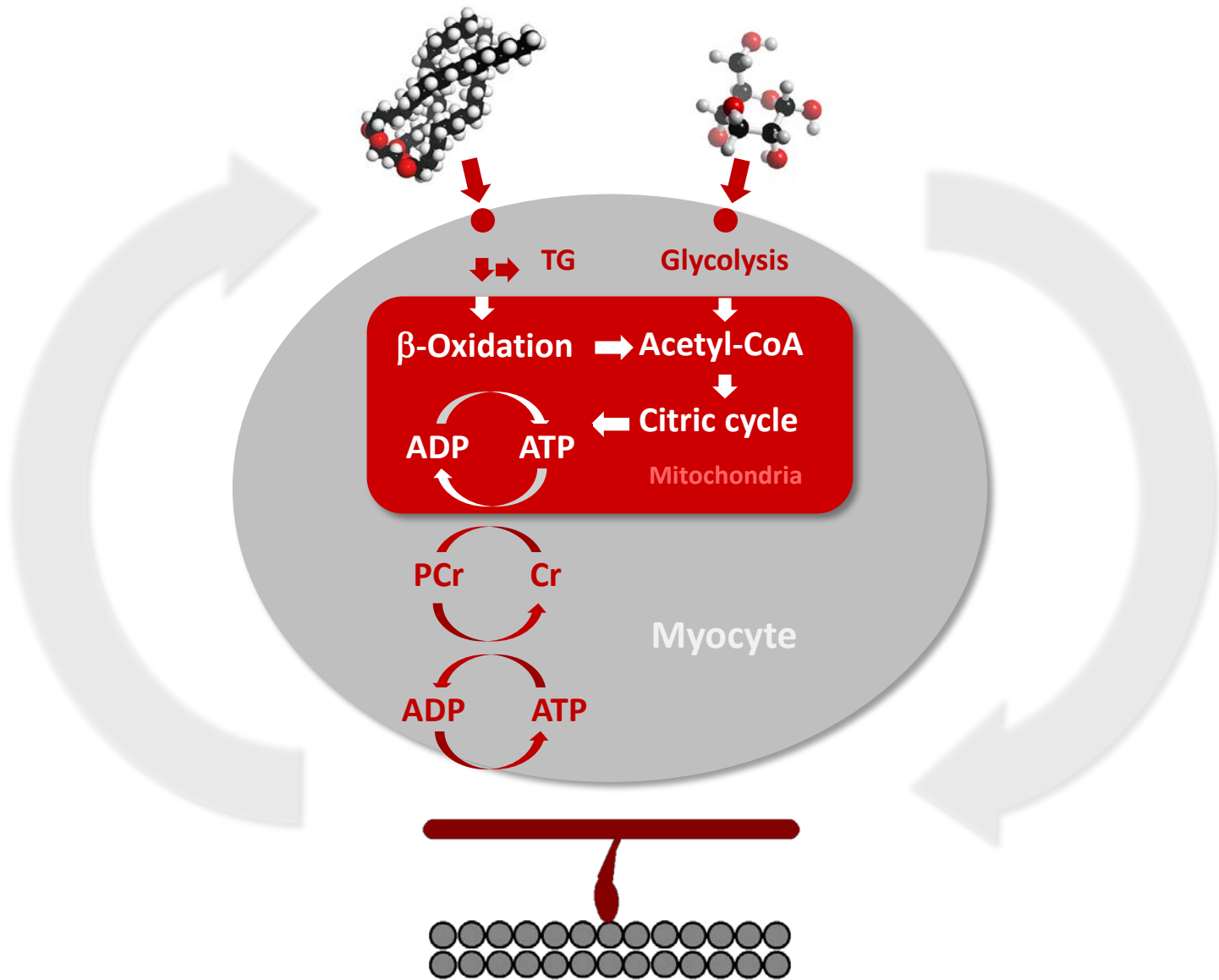
Frequency → Chemical Shift



Chemical shift



Cell respiration



Spectroscopy

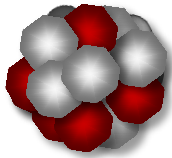
Radio transmitter



Position → Frequency



Signal source



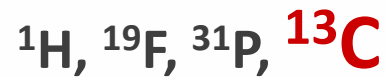
Radio receiver



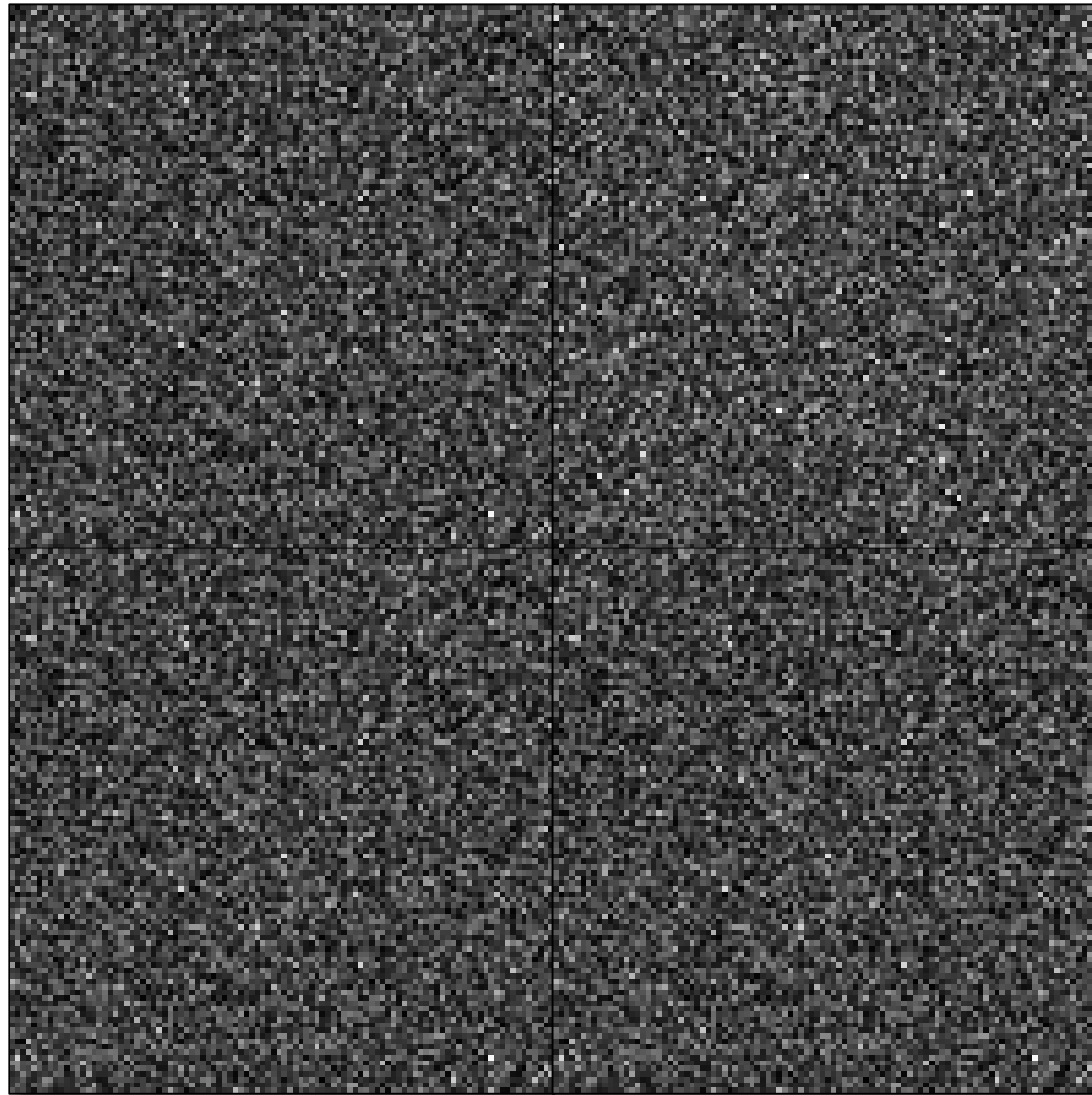
Magnetic field



Frequency → Position

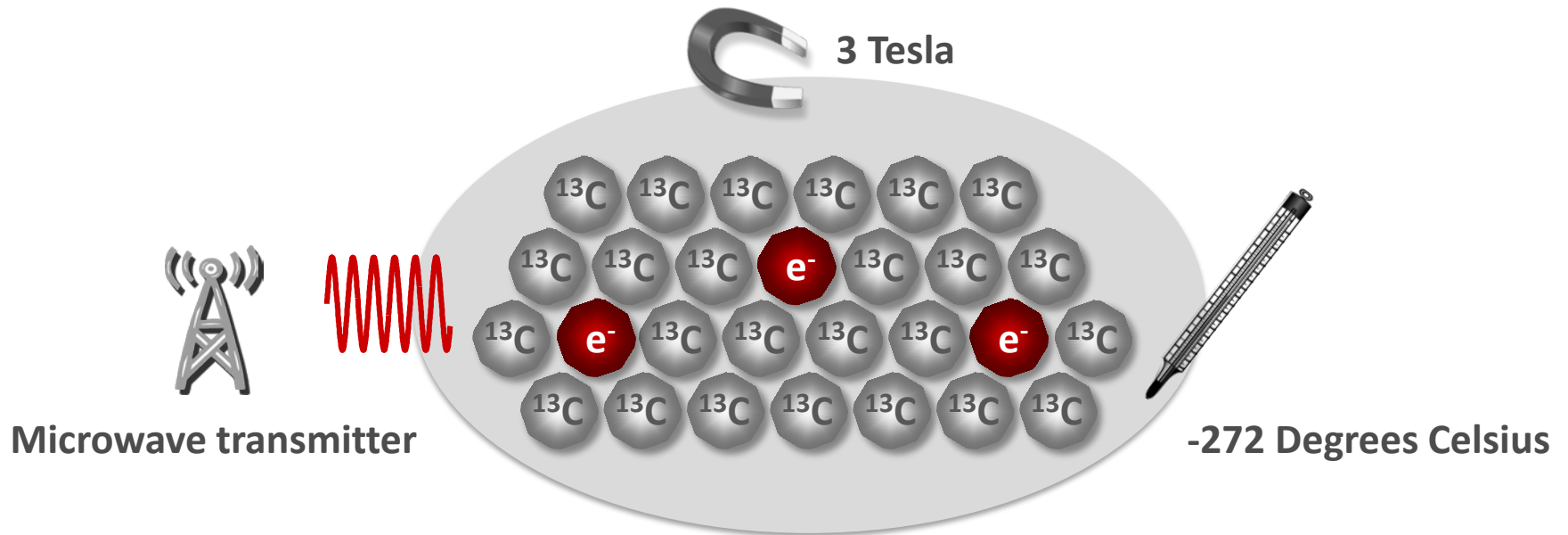
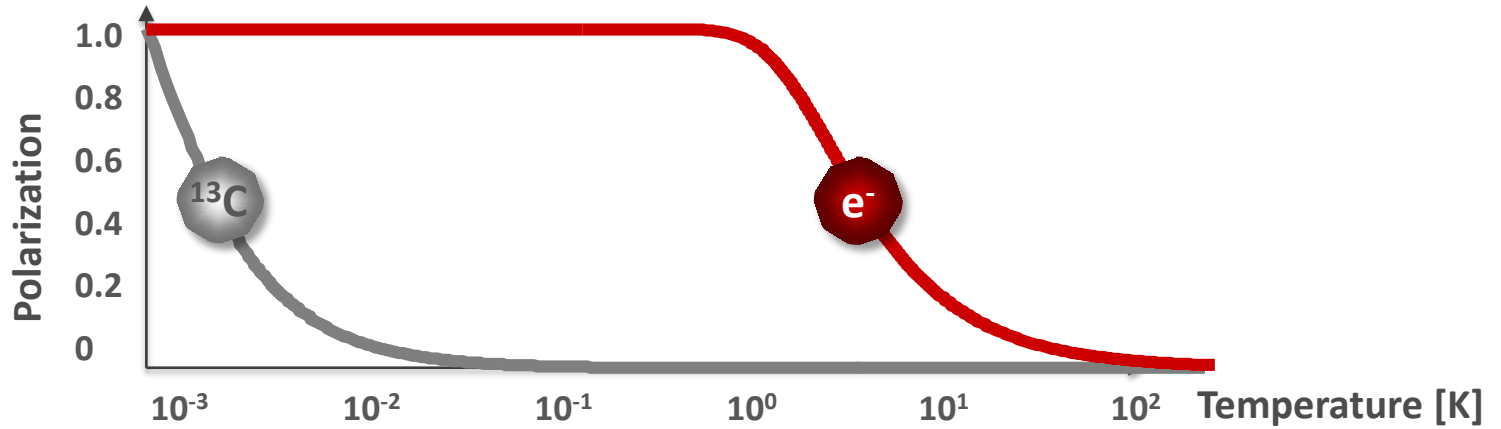


Carbon imaging

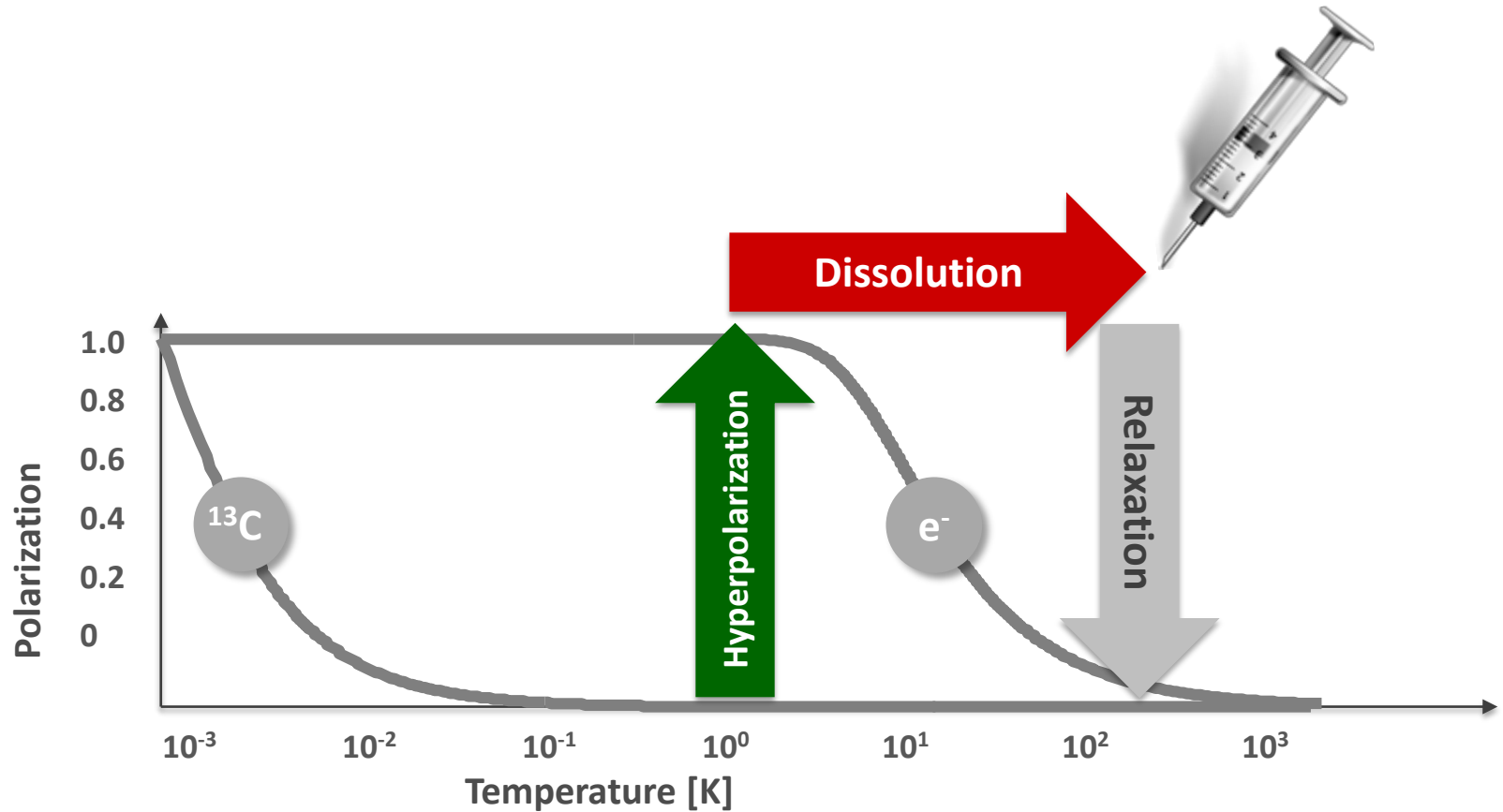


0.1-1 mM

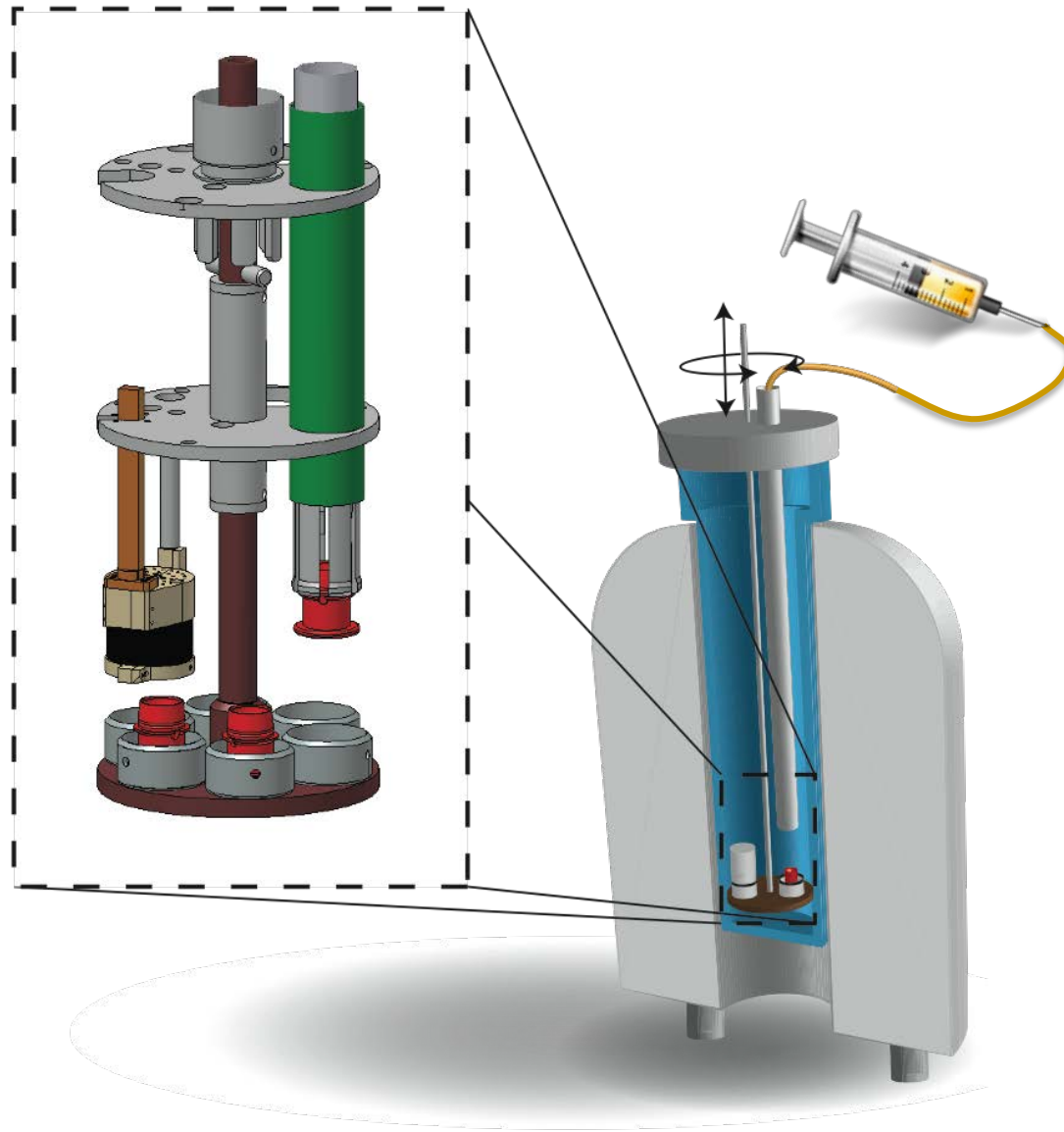
Dynamic Nuclear Polarization



Dissolution Dynamic Nuclear Polarization



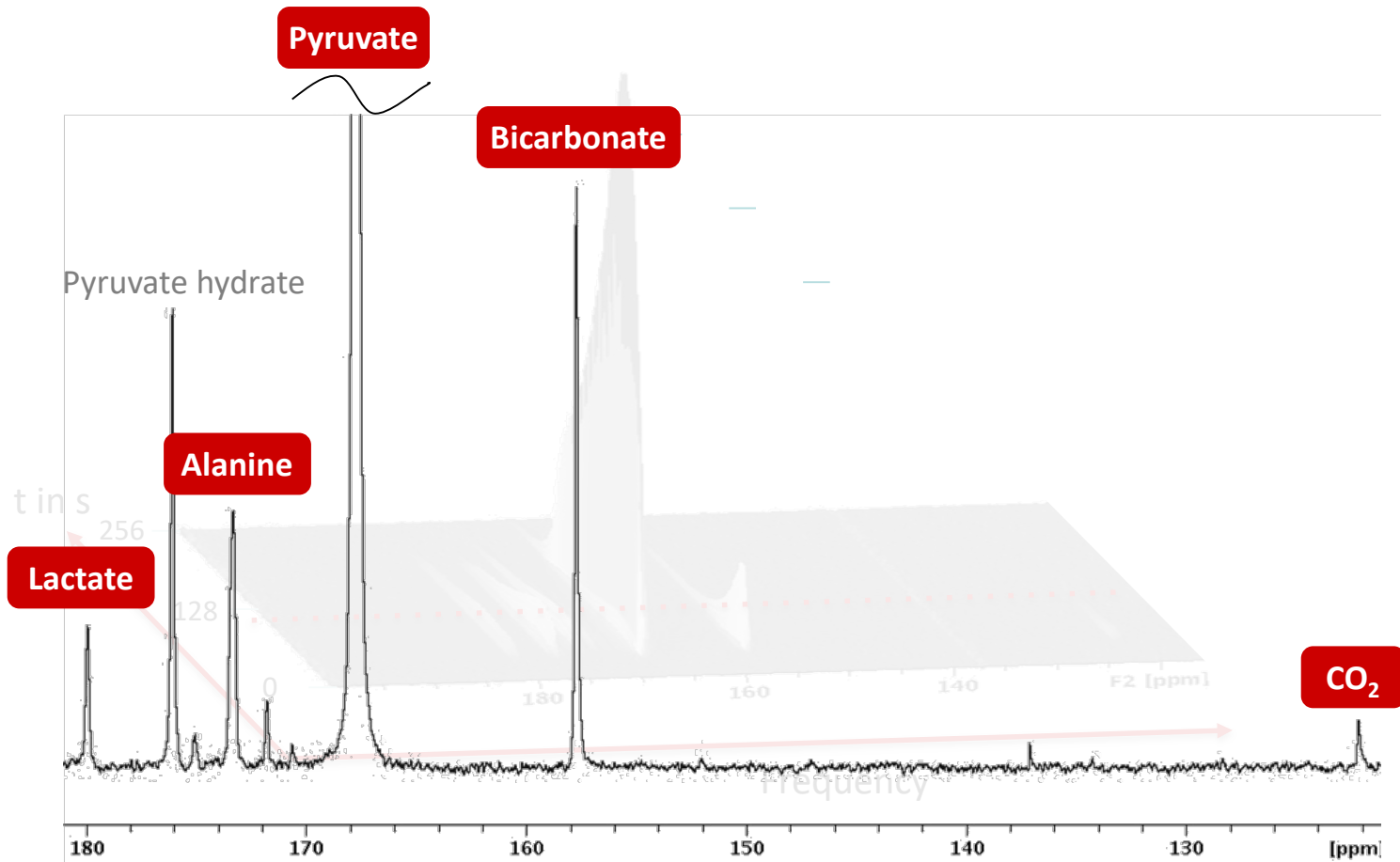
Prototype polarizer



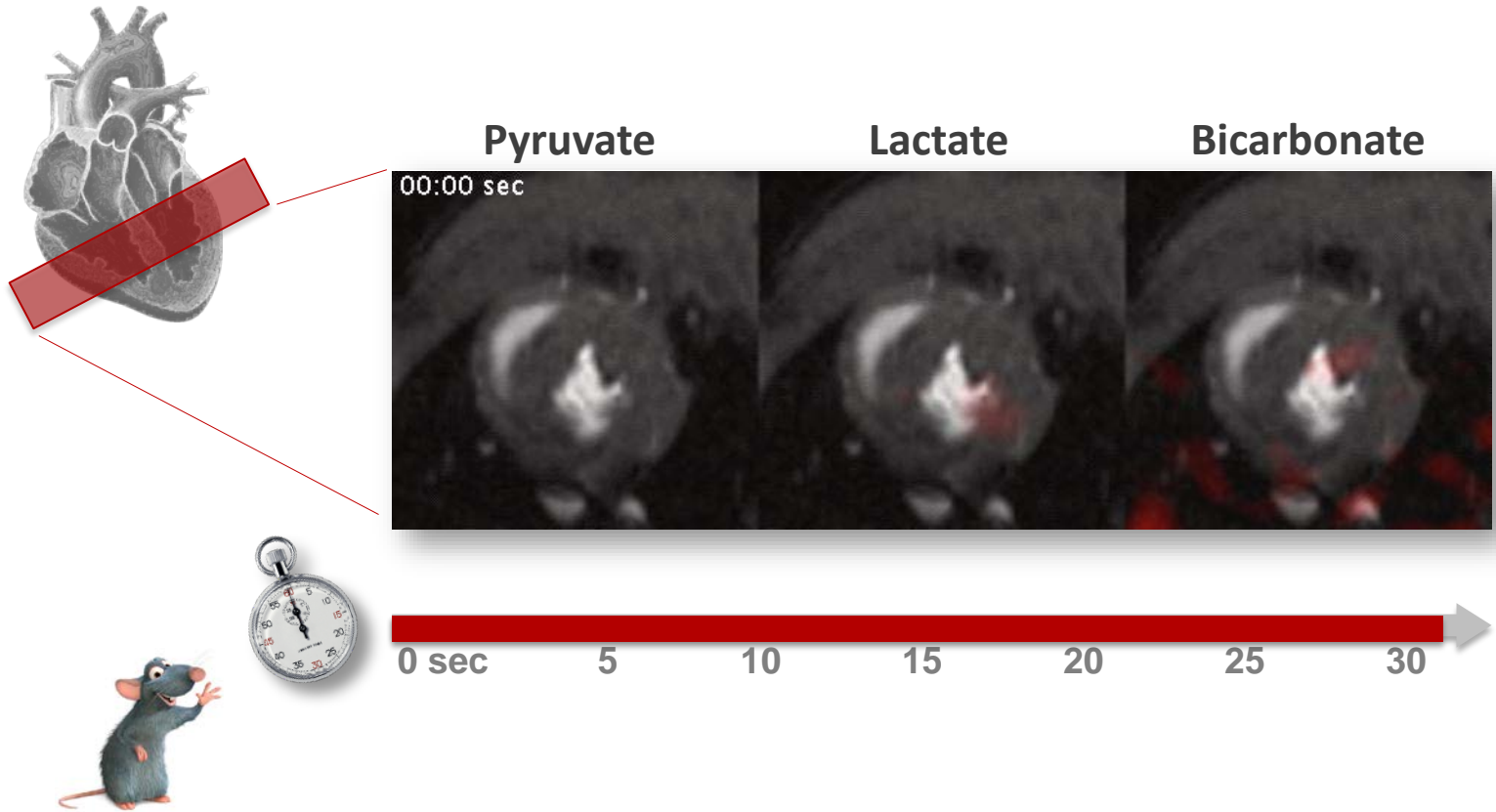
Dissolution dynamic nuclear polarization



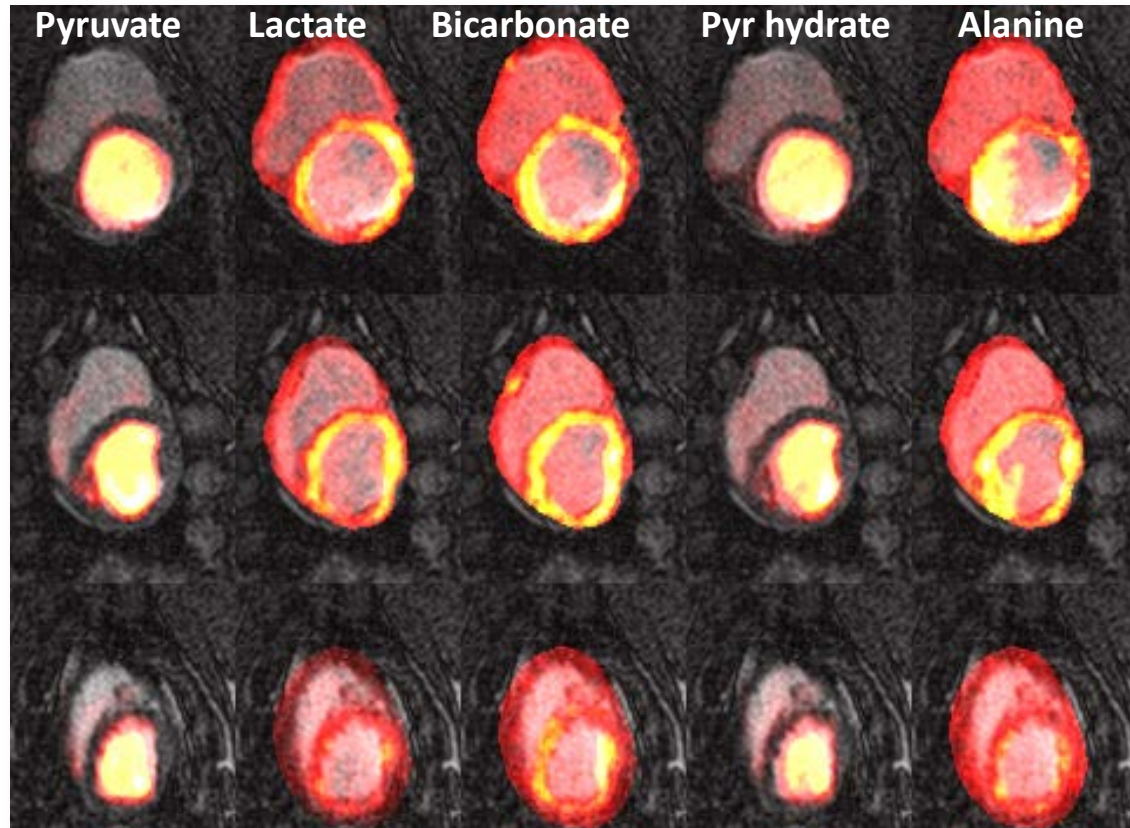
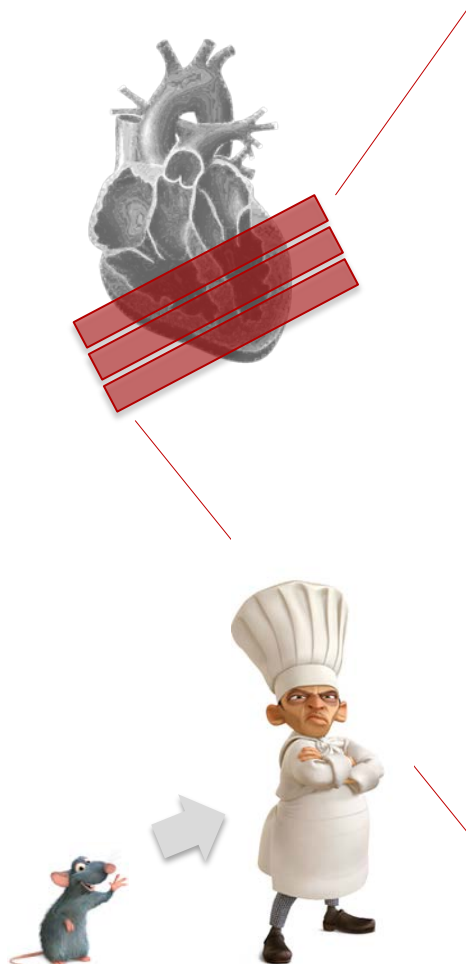
Metabolism of isolated rat heart



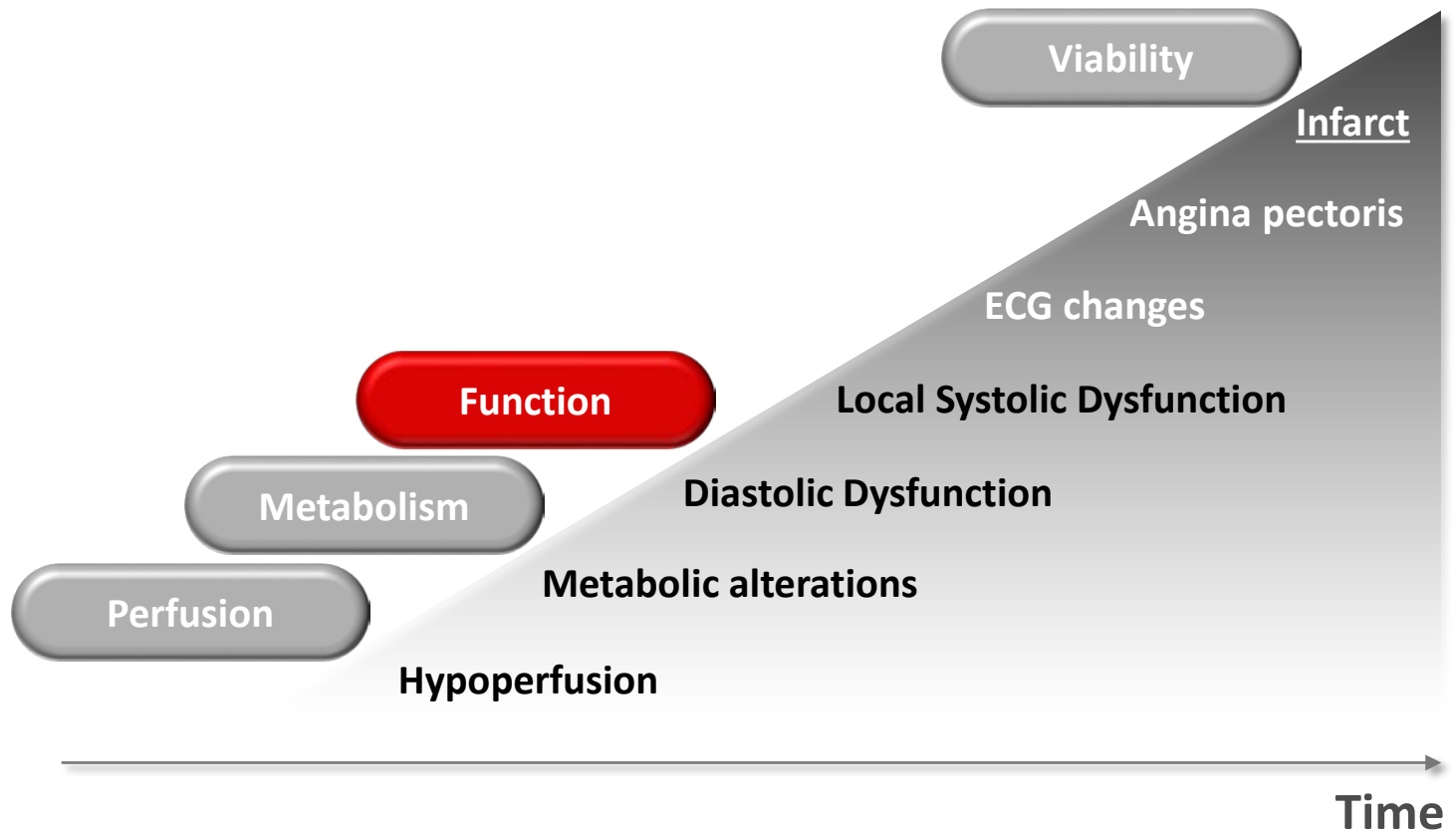
Real-time metabolic imaging



From bench to bedside



Ischemic cascade



Blood flow

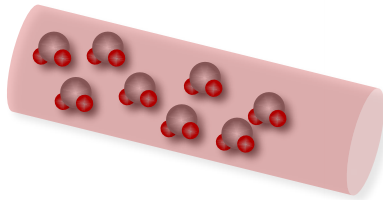
Radio transmitter



Velocity → Phase



Signal sources



Radio receiver



Magnetic field

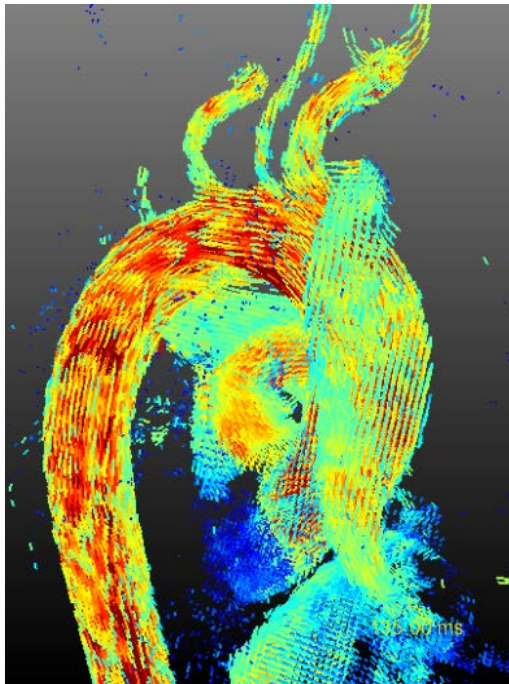


Phase → Velocity

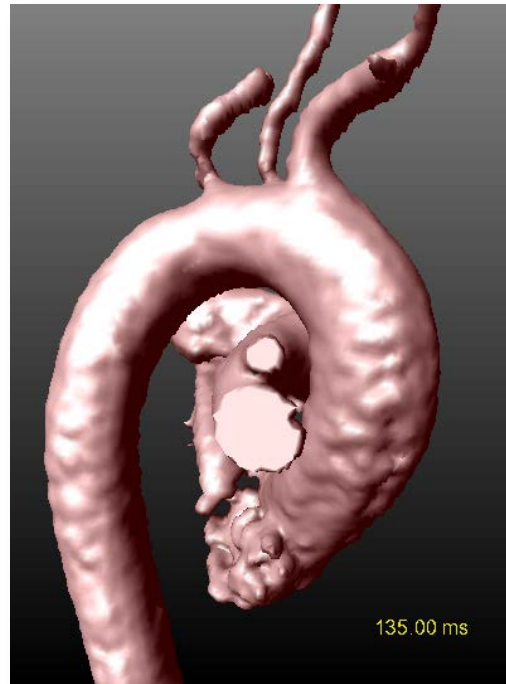


Blood flow quantification – relative pressure maps

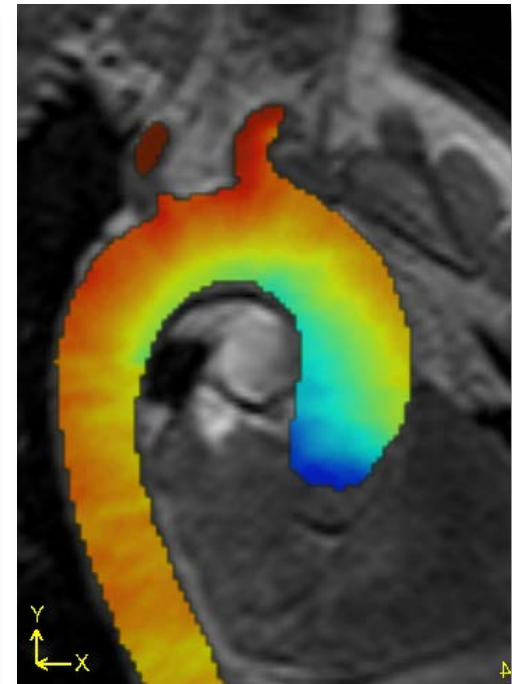
Flow field



Boundaries

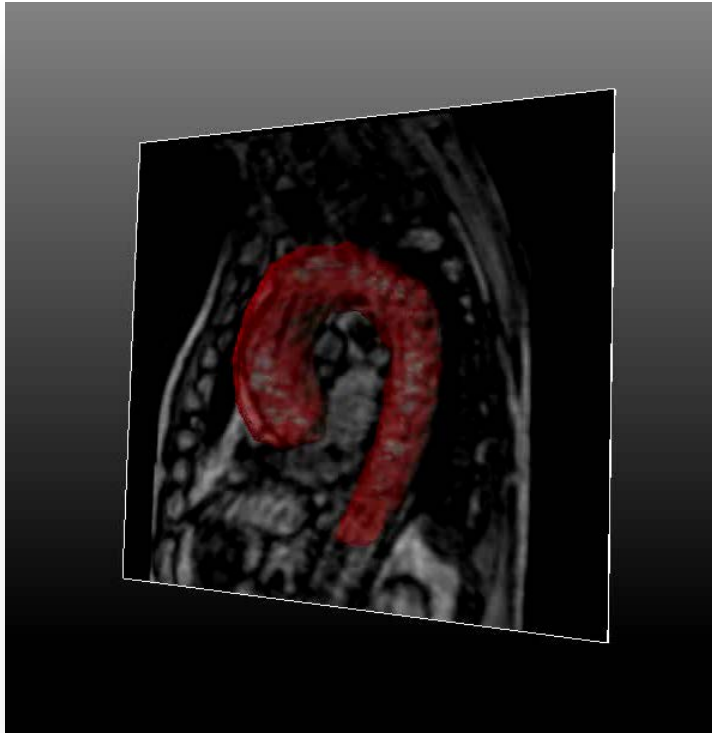


Pressure field

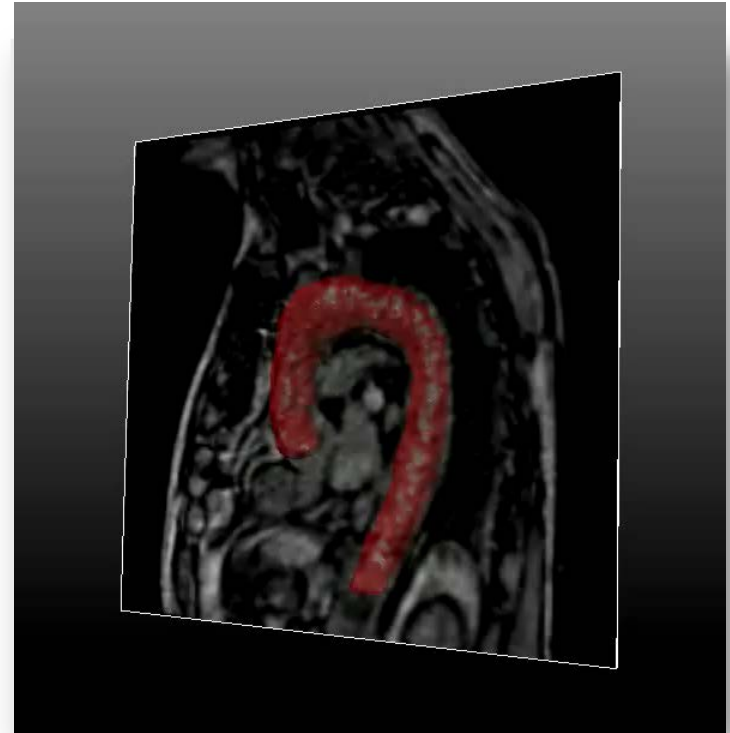


Blood flow quantification

Pre operation

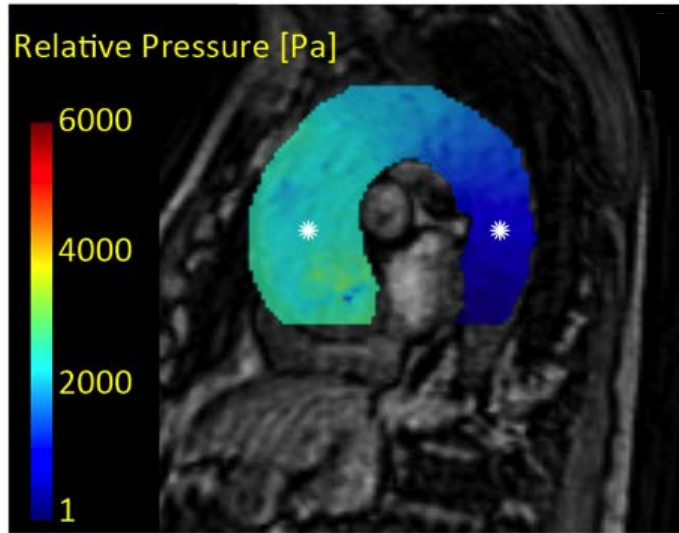


Post operation

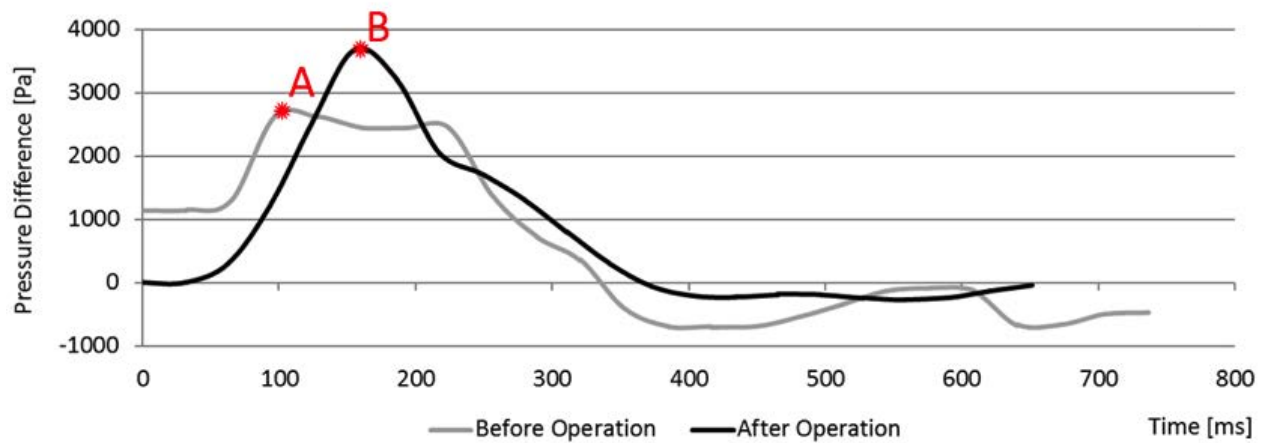
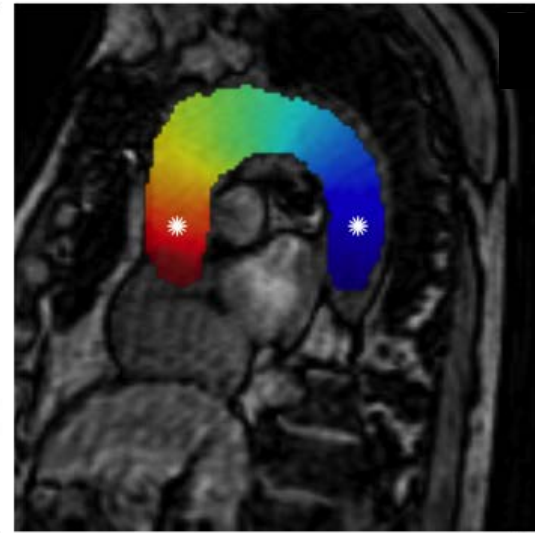


Blood flow quantification

Pre operation



Post operation



Diffusion

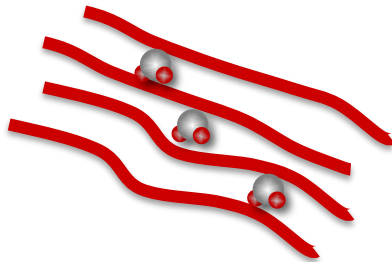
Radio transmitter



Position → Frequency



Signal sources



Magnetic field



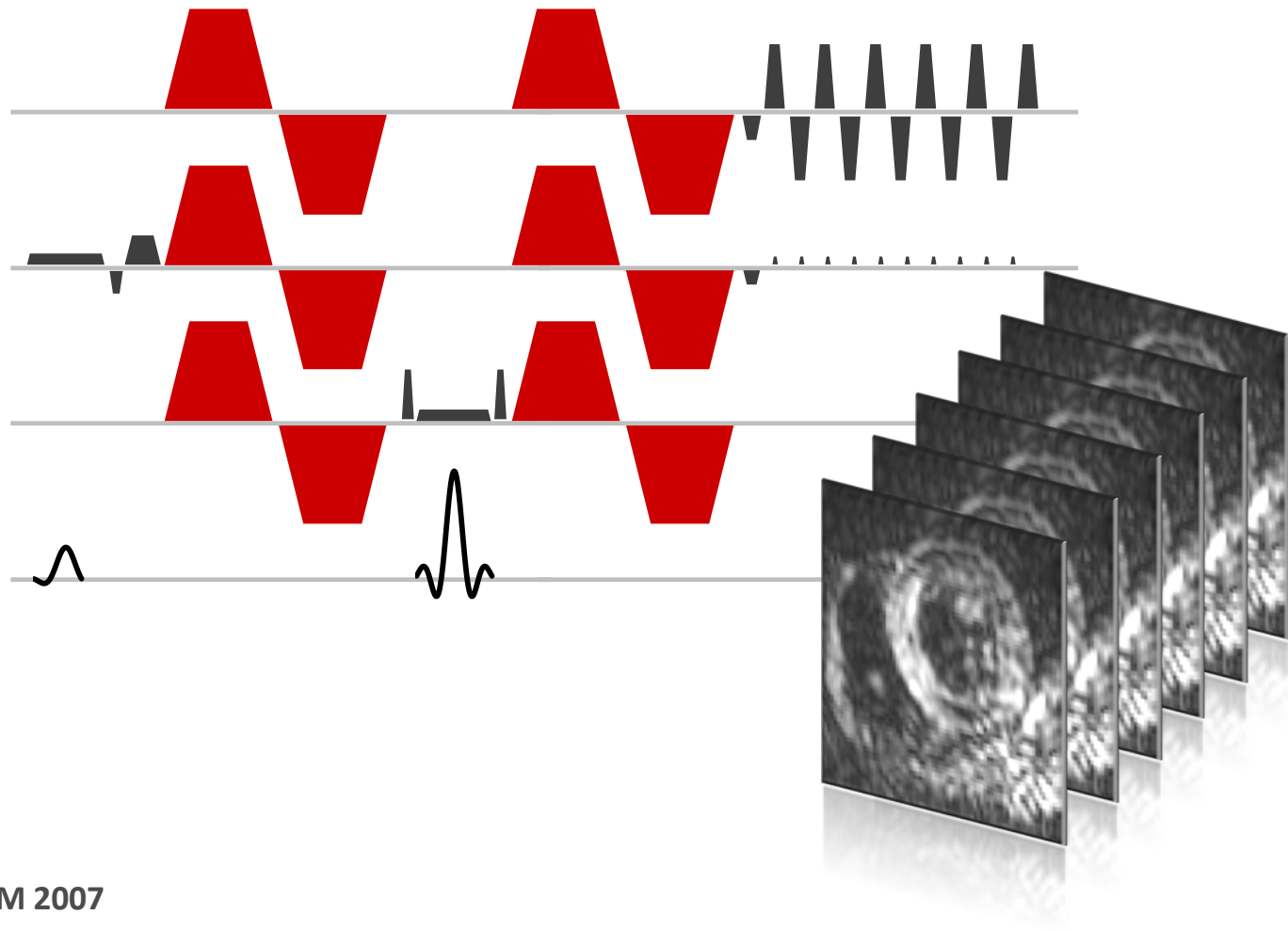
Radio receiver



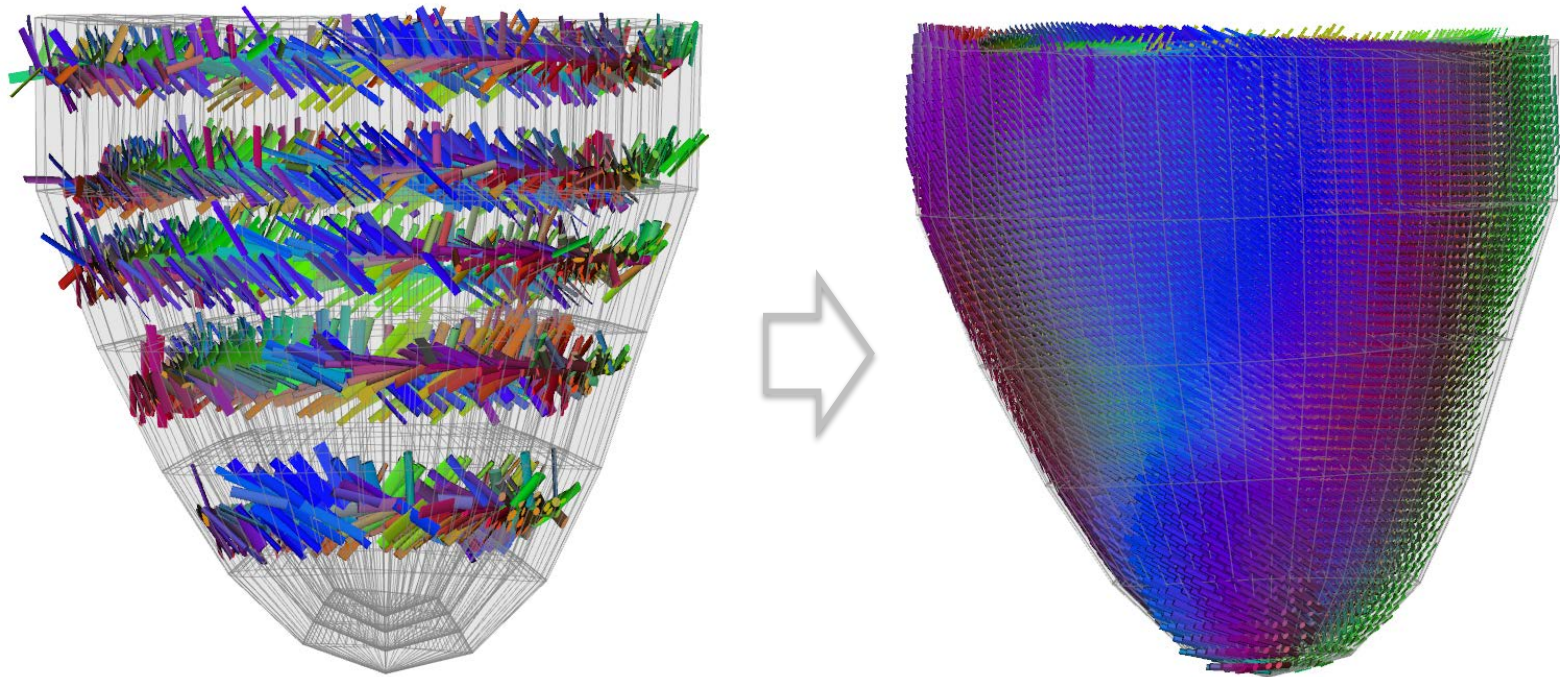
Frequency → Position



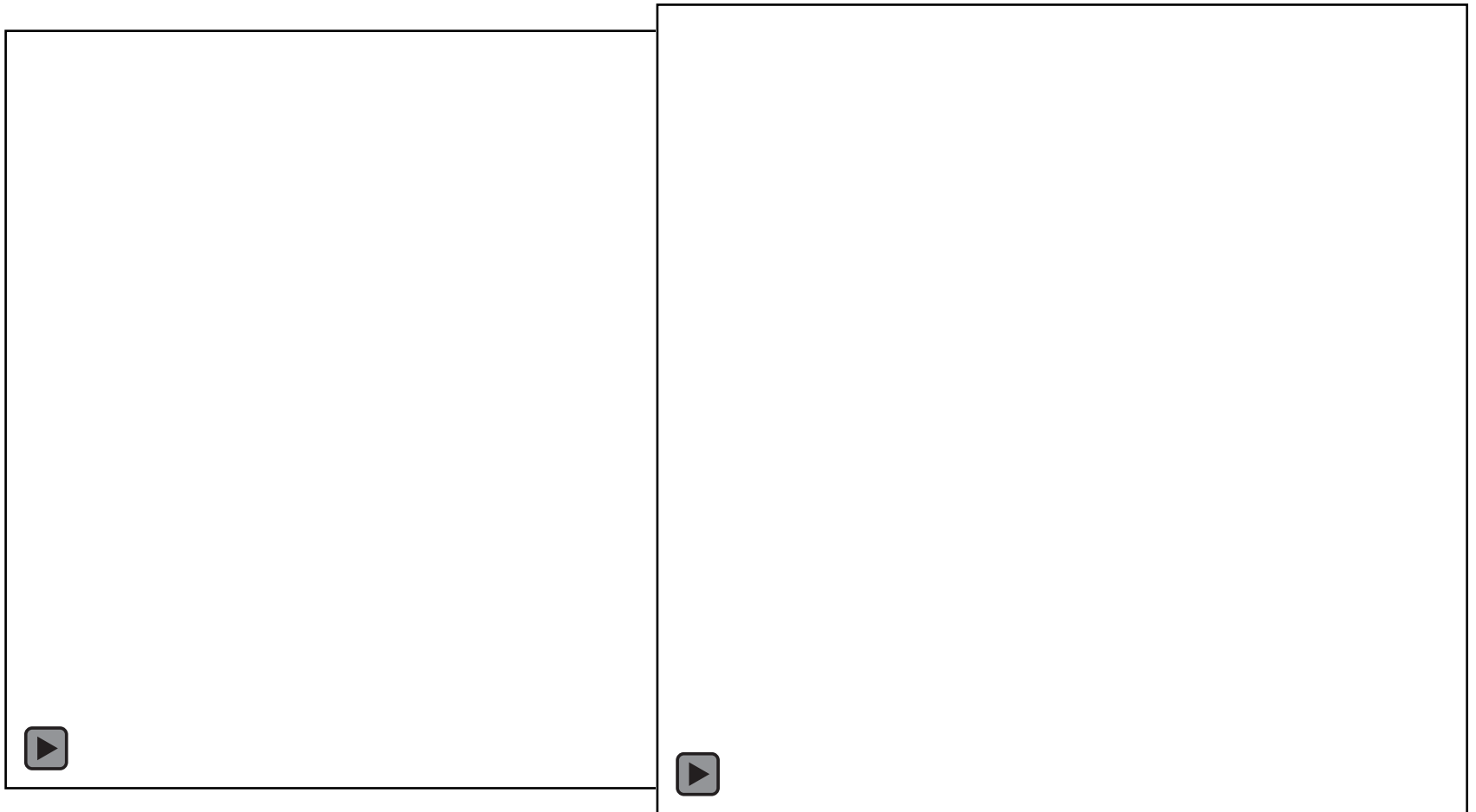
Velocity compensated diffusion-weighted spin-echo



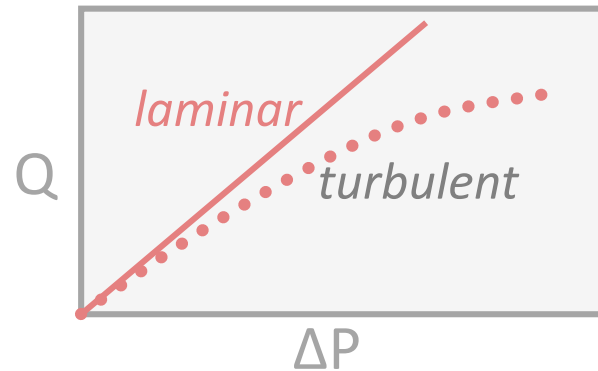
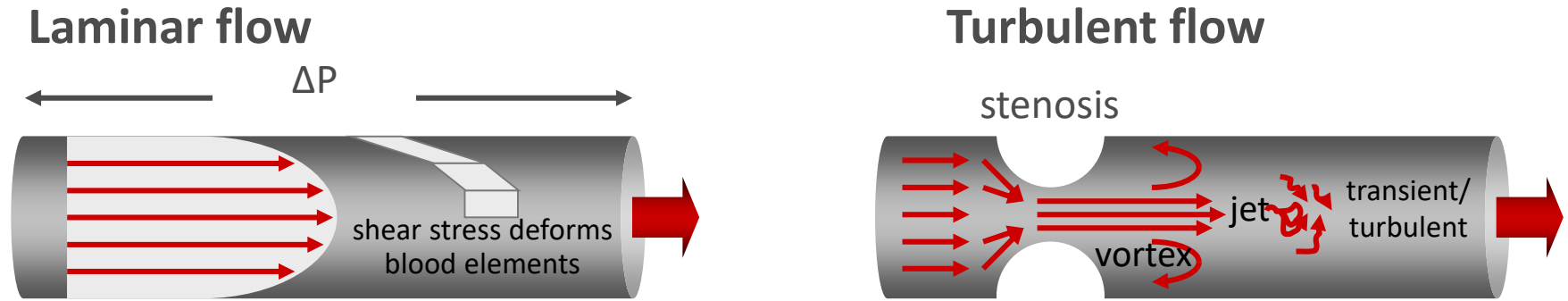
Conformal mapping



Dynamic Diffusion Tensor Imaging

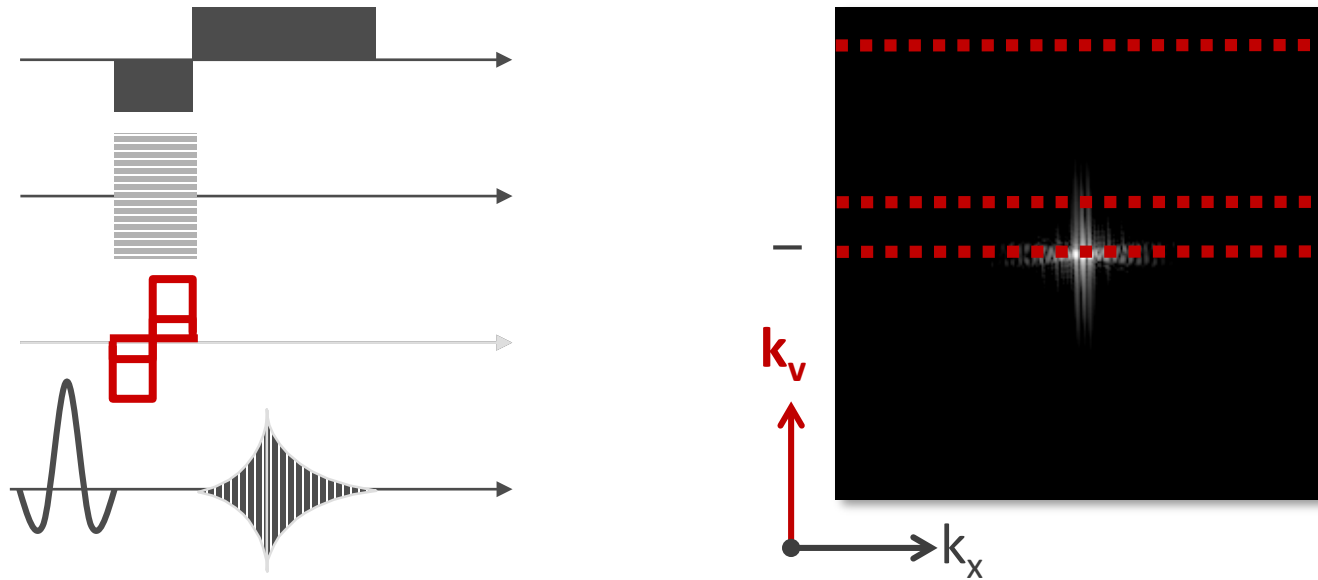


Laminar and turbulent flows

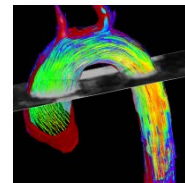
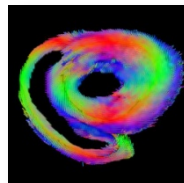


$$\text{ReynoldsNumber} = \frac{\rho v d}{\mu} \propto \frac{\text{Inertial force}}{\text{Viscous force}}$$

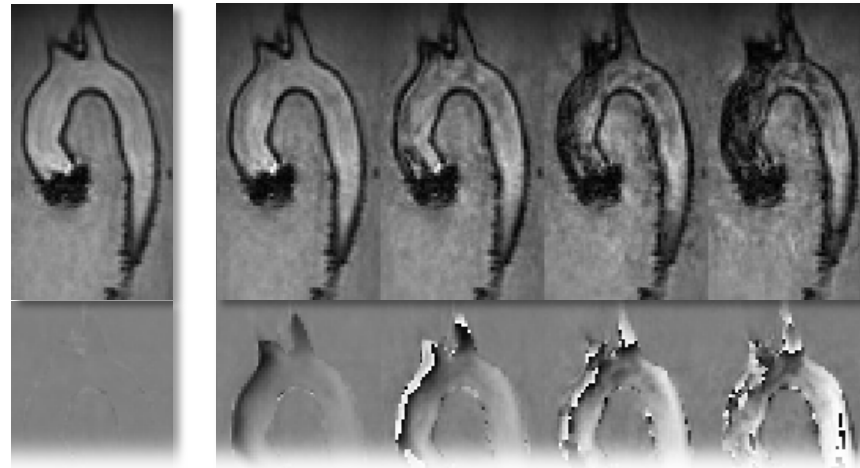
Universal signal model



$$S(k_v) = S_0 e^{-\frac{\sigma_v^2 k_v^2}{2}} e^{i(vk_v + \varphi)}$$



Bayesian parameter estimation



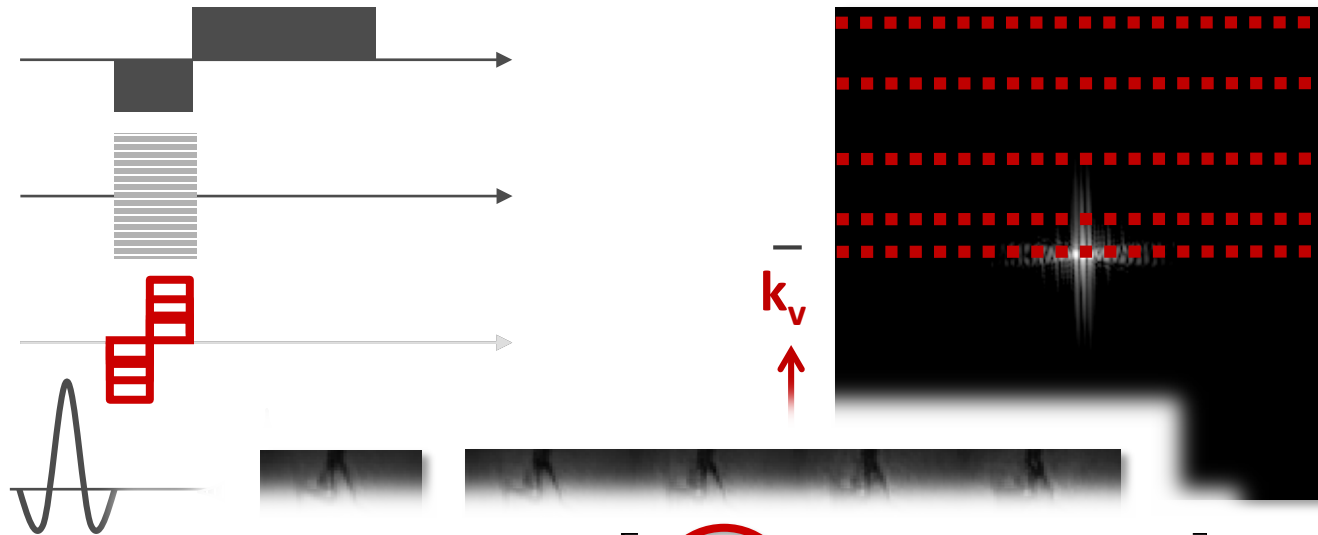
$$P(\Theta, \mathbf{B} | M, I) = \frac{P(\Theta, \mathbf{B} | I) P(M | \Theta, \mathbf{B}, I)}{P(M | I)} \quad \Theta = [\sigma, v]$$

$\int \int d\sigma_n d\mathbf{B}$

$\boxed{P(\Theta | M, I)}$

Incorporate bounds of parameters Incorporate knowledge about the noise

Bayesian multi-point velocity encoding



$$\text{Re} = \begin{bmatrix} \delta_{xx} & \tau_{xy} & \tau_{xz} \\ \tau_{yx} & \delta_{yy} & \tau_{yz} \\ \tau_{zx} & \tau_{zy} & \delta_{zz} \end{bmatrix} = \rho \begin{bmatrix} \langle v_1'^2 \rangle & \langle v_1' v_2' \rangle & \langle v_1' v_3' \rangle \\ \langle v_1' v_2' \rangle & \langle v_2'^2 \rangle & \langle v_2' v_3' \rangle \\ \langle v_1' v_3' \rangle & \langle v_2' v_3' \rangle & \langle v_3'^2 \rangle \end{bmatrix}$$

$$\text{TKE} = \frac{\rho}{2} \sum_{i=1}^3 \langle v_i'^2 \rangle = \frac{\rho}{2} \sum_{i=1}^3 \sigma_i^2$$

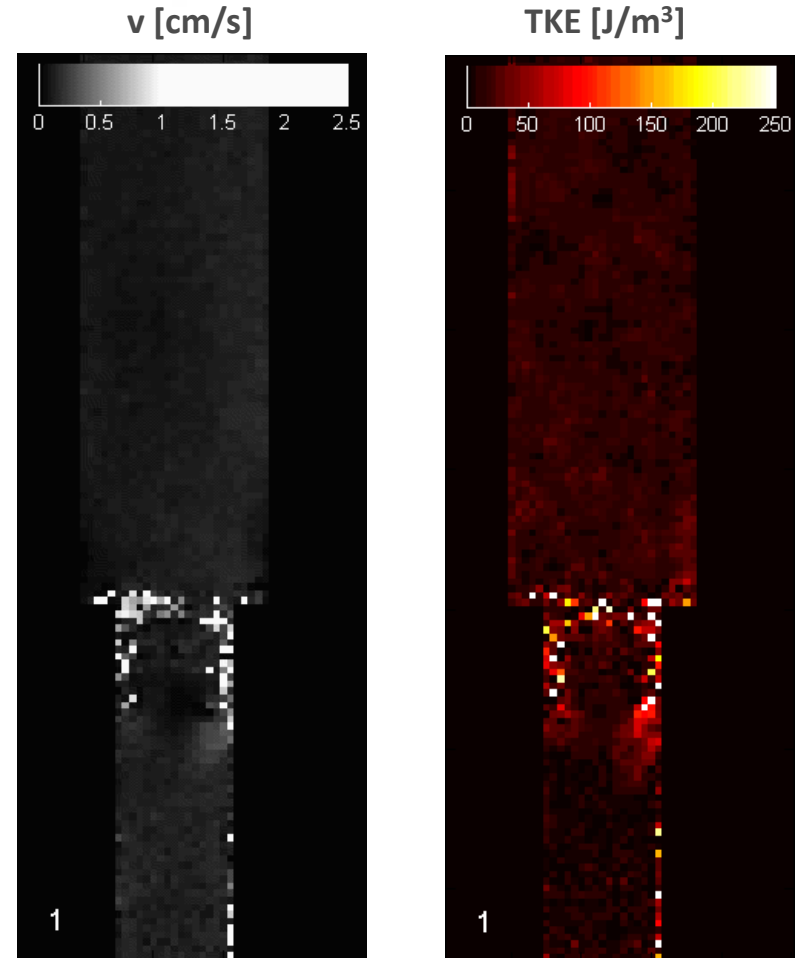
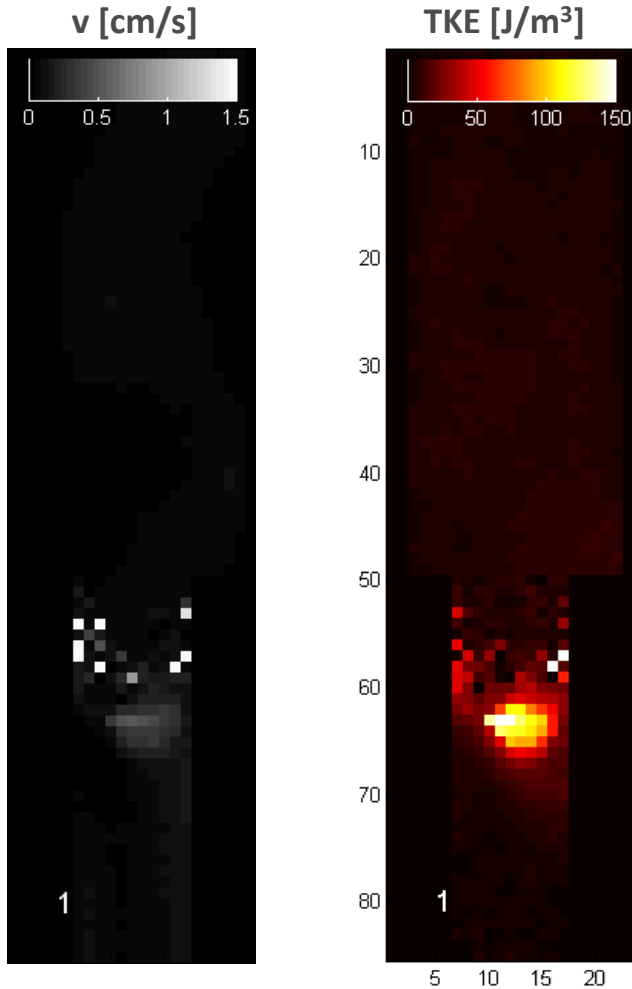
Aortic valves in-vitro



St. Jude Medical®

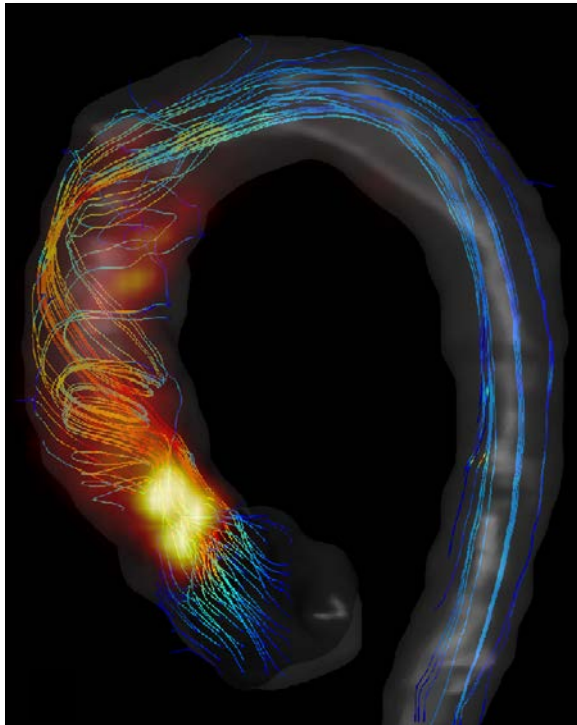


Edwards® Sapien



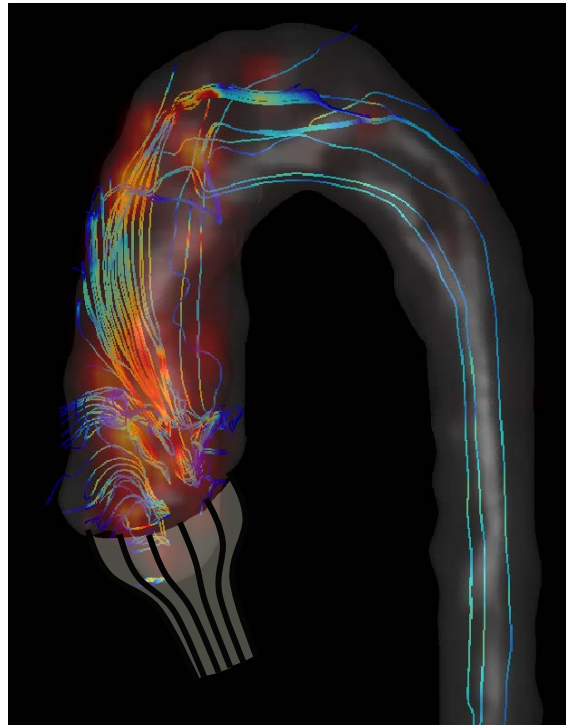
Aortic valves in-vivo

Aortic Stenosis



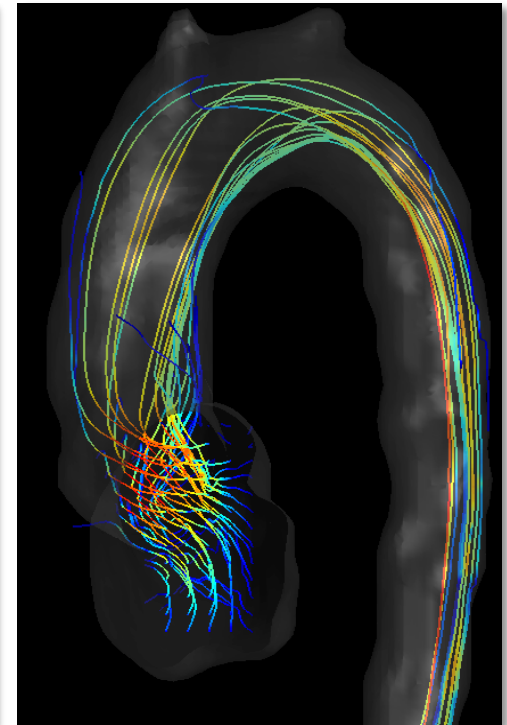
TKE_{peak} **940 J/m³**
 V_{peak} **3.3 m/s**

TAVI

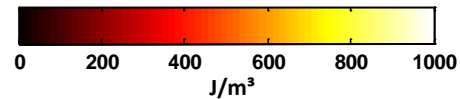
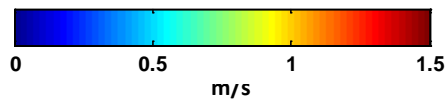


TKE_{peak} **540 J/m³**
 V_{peak} **2.4 m/s**

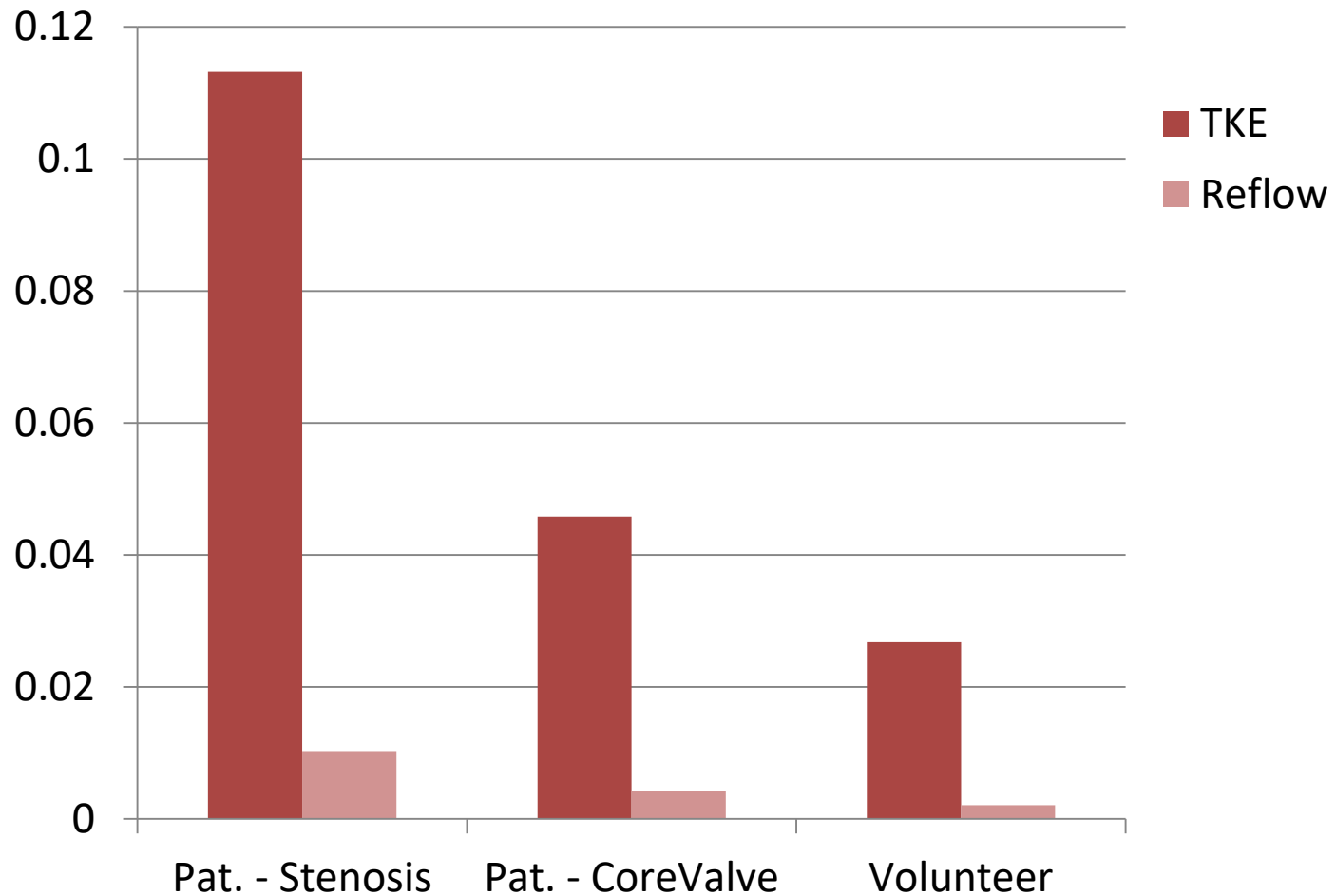
Healthy



TKE_{peak} **150 J/m³**
 V_{peak} **1.3 m/s**



Energy Loss index



Energy Loss index

$$ELi = \left(\frac{TKE \cdot \text{voxelsize}_{z\text{-dir.}} + RF}{MKE} \right) \cdot \frac{1}{1 - RF}$$

Image guided simulations

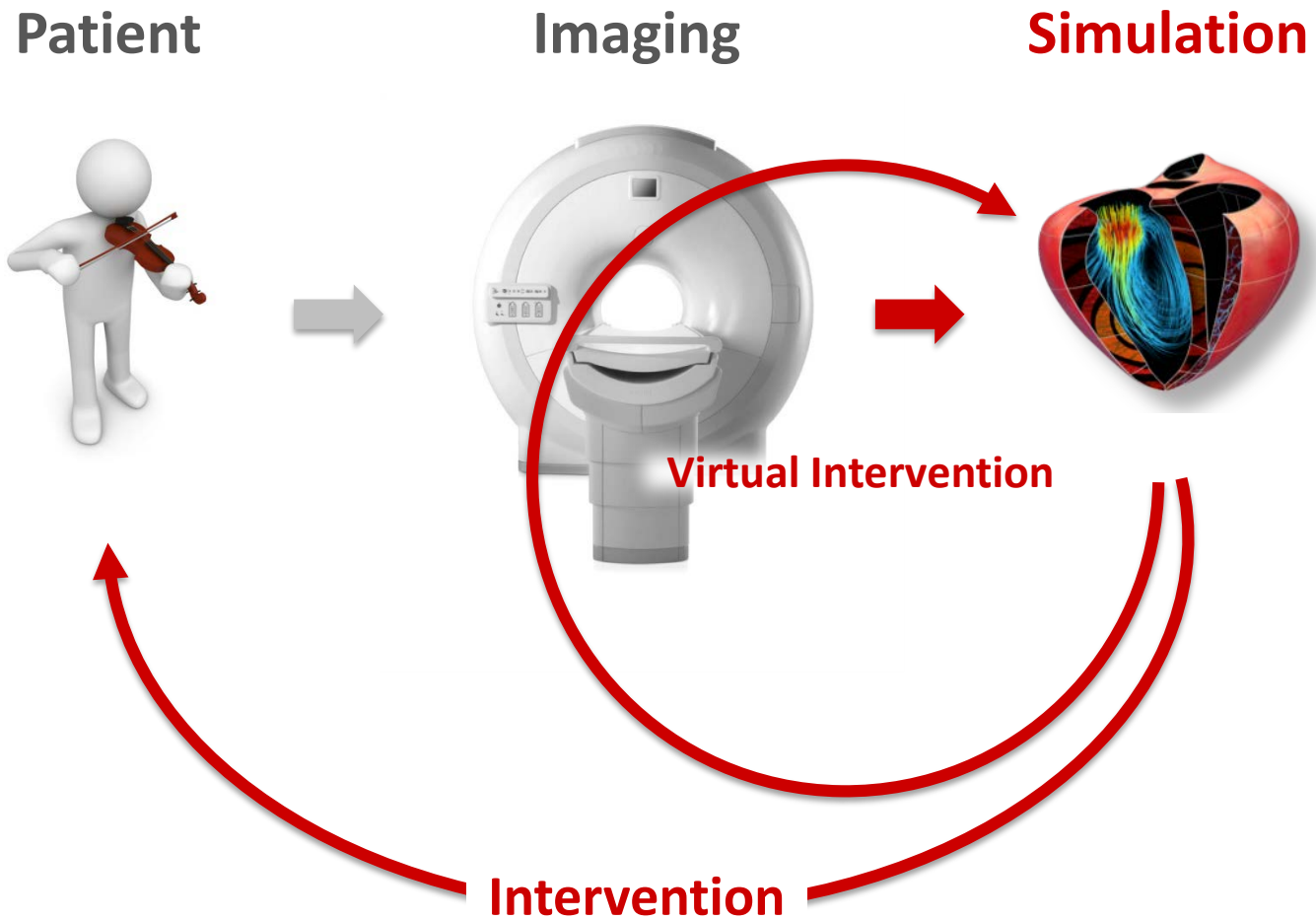
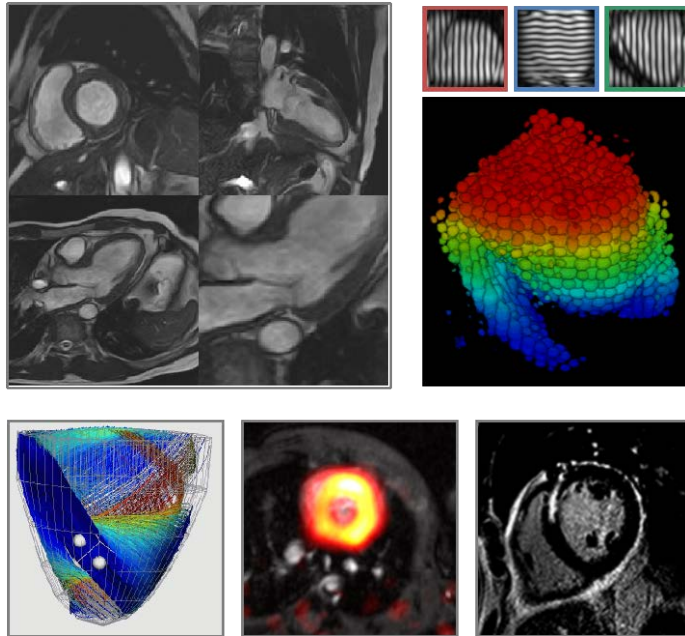
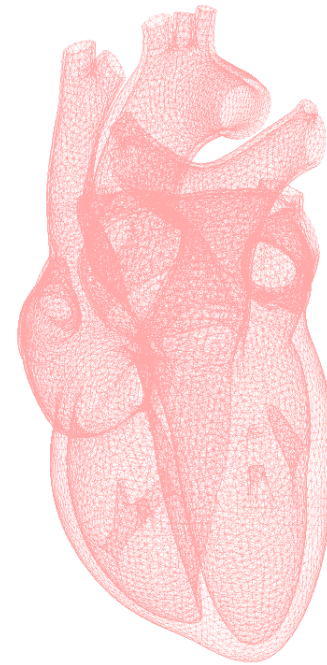


Image-guided modeling and prediction

In-vivo measurements

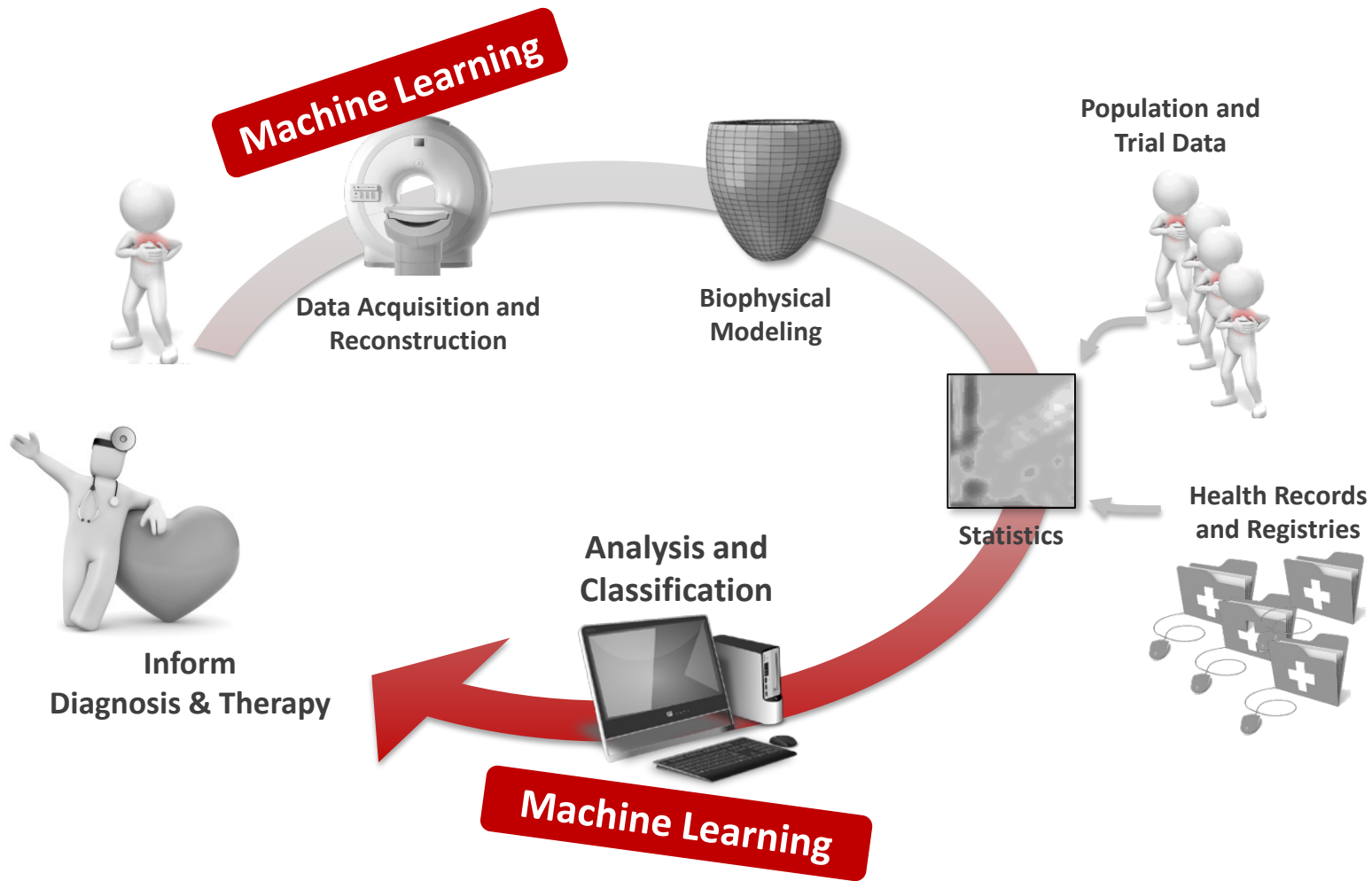


In-silico prediction



90 days

Big Data Processing



Acknowledgements

University and ETH Zurich

- Christian Stoeck
- Patrick Wespi
- Johannes Schmidt
- Verena Knobloch
- Max Fuetterer
- Julia Busch
- Lukas Wissmann
- Christian Binter
- Rudolf Fischer
- Michael Batel
- Marcin Krajewski
- Matthias Ernst
- Martin Buehrer
- Gerard Crelier
- Klaas Pruessmann

King's College London

Daniel Giese
Claudio Santelli
Constantin von Deuster
Darach O'h-ici
Nicolas Toussaint
Sven Plein

University Hospital Zurich

Robert Manka
Markus Niemann

Funding

SNF
KTI/CTI
EU FP7
EPSRC
PHILIPS